

# Direccionalidad de los fotorreceptores, su función en visión y en diagnósticos

Understanding photoreceptor directionality in vision and diagnostics



**Brian Vohnsen**

Advanced Optical Imaging Group  
University College Dublin, Irlanda



# Structure and optics of the human eye

## Cornea

- ~ 43 dioptres
- ~ 1.376 refractive index

## Lens

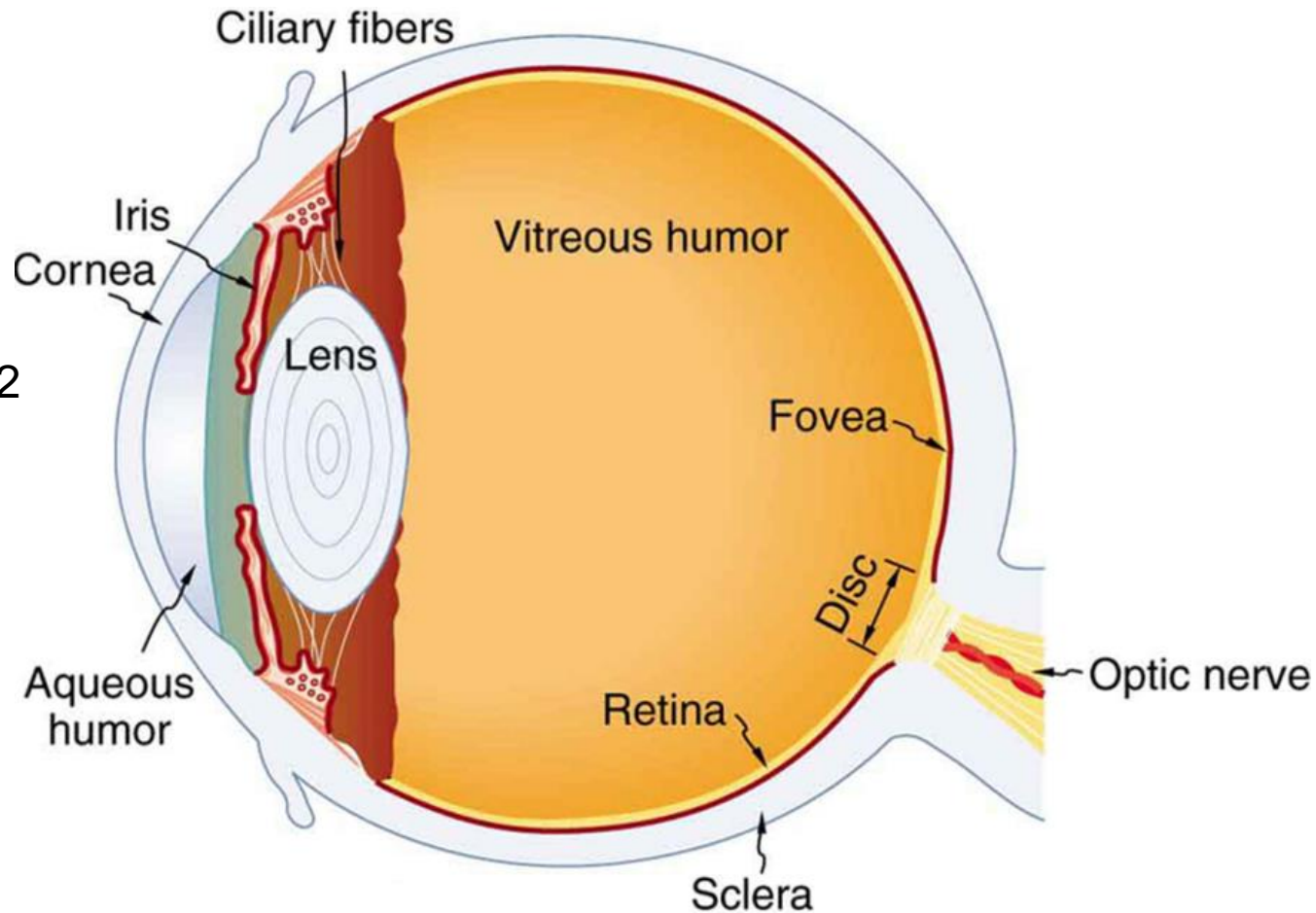
- ~ 18 dioptres
- ~ Graded index 1.37-1.42

## Axial length

22 – 25 mm (or higher)

## Retina

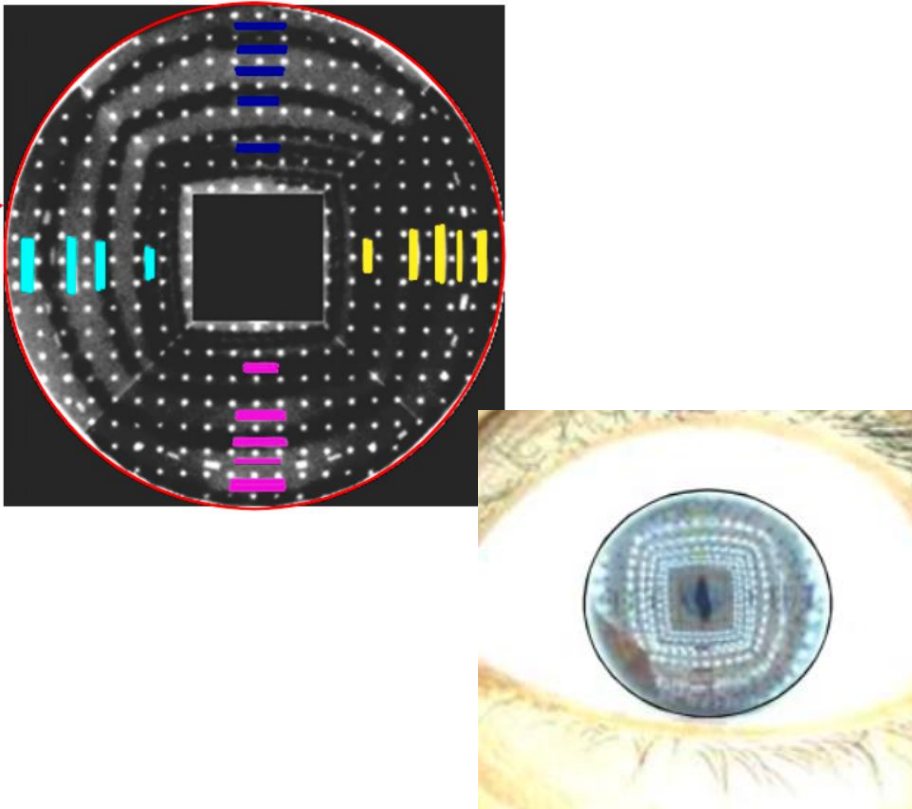
- ~ 70%
- ~ 6M cones (S,M,L)
- ~ 90M rods



# Corneal and ocular aberrations

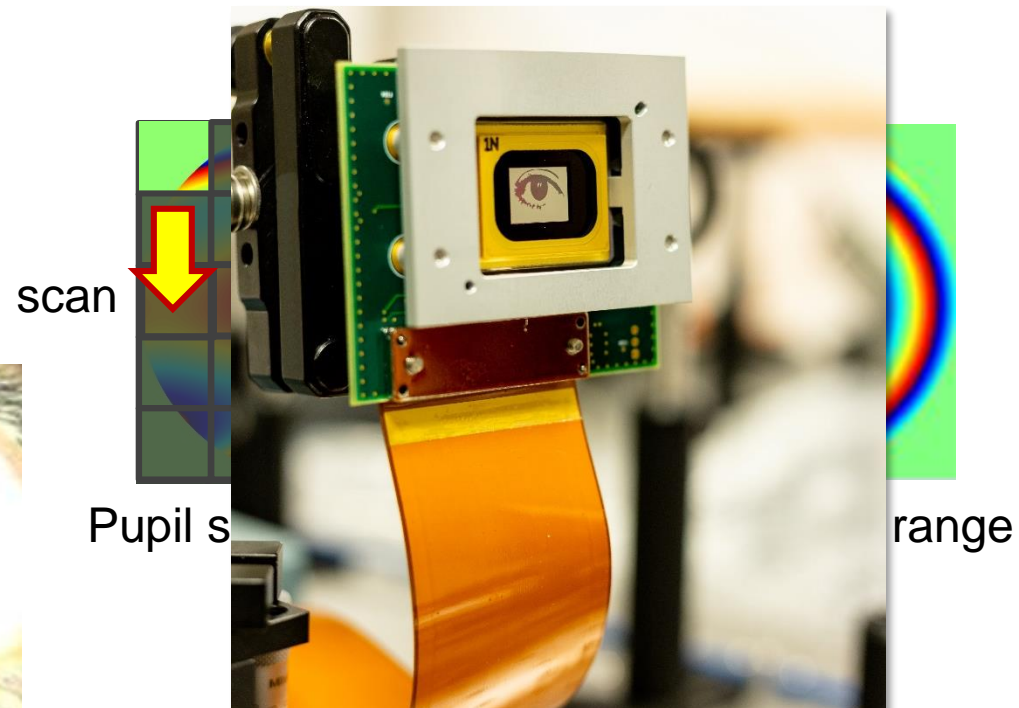
Null-screen corneal aberrometry

With M. Rodríguez-Rodríguez



Hartmann-Shack ocular wavefront sensing without crosstalk

With A. Carmichael Martins



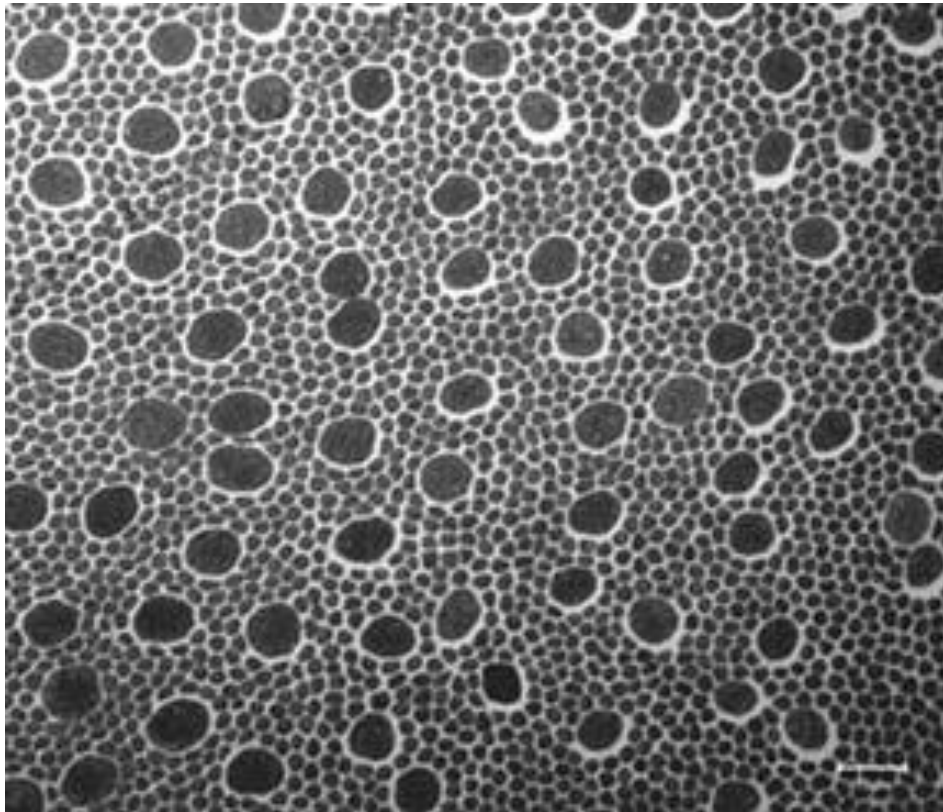
ARVO 2019 + poster MyT2019-123

*Manuscript in preparation*

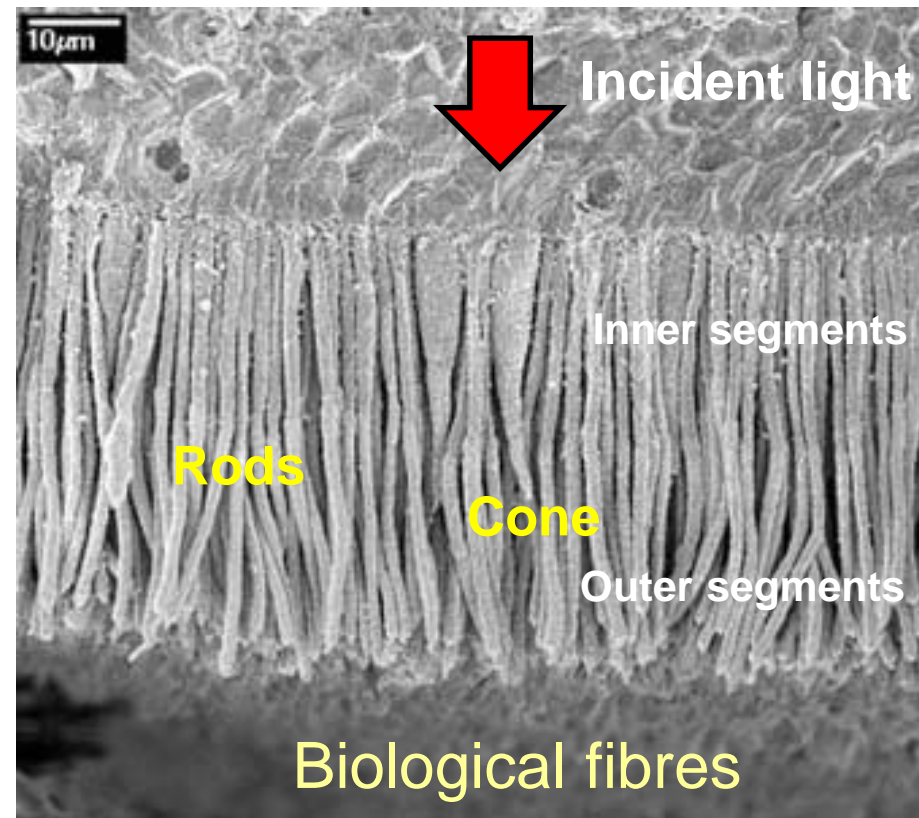
- B. Vohnsen et al., Appl. Opt. 2018
- A. Carmichael and B. Vohnsen, Micromachines 2019

# Cones and rods of the human retina

**En-face** view of parafovea cones and rods



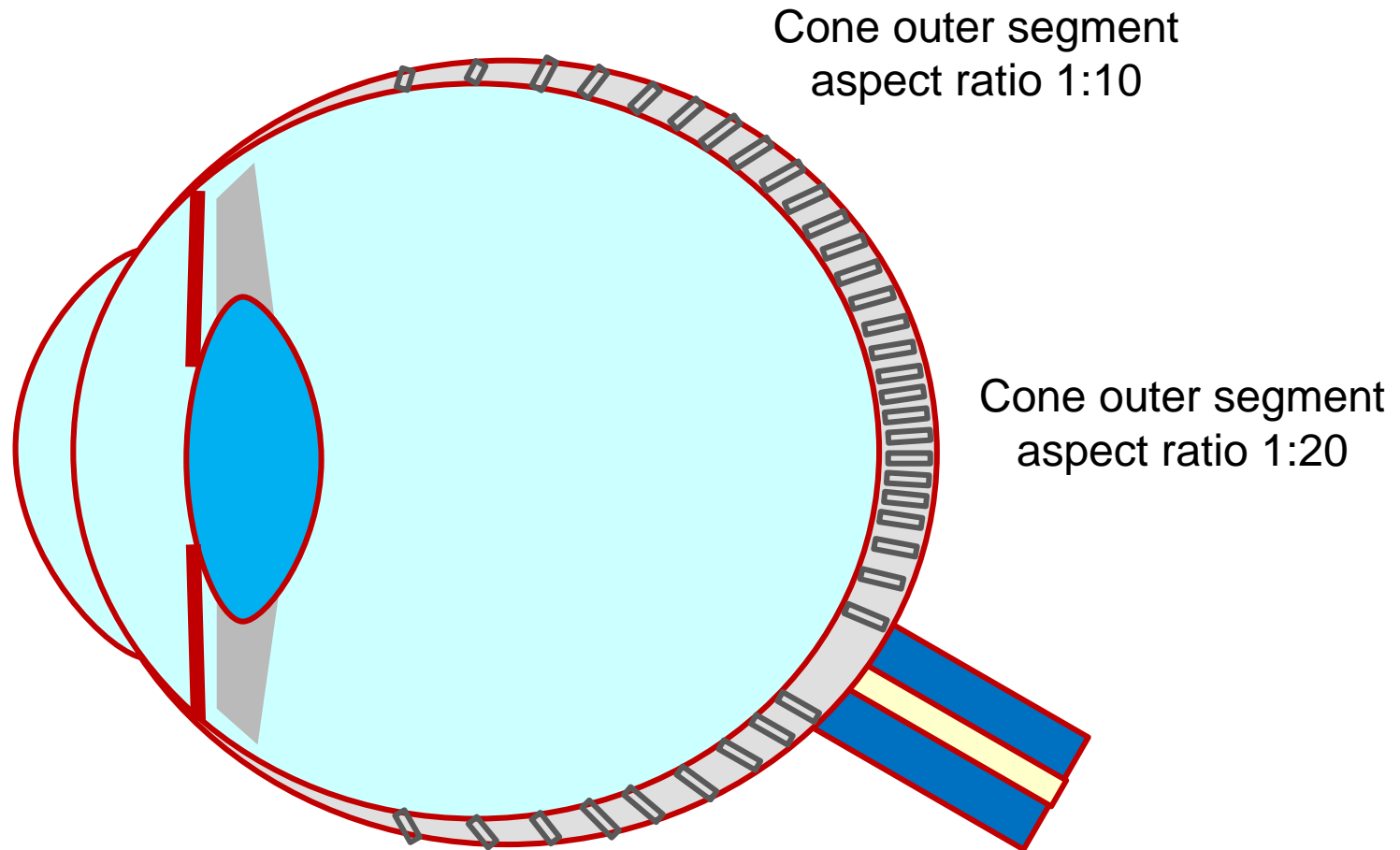
**Side view** of parafovea cones and rods



Cone photoreceptor diameter ranging from about 2  $\mu\text{m}$  (fovea) to 8  $\mu\text{m}$  (parafovea)

Images by courtesy of P. Munro, UCL

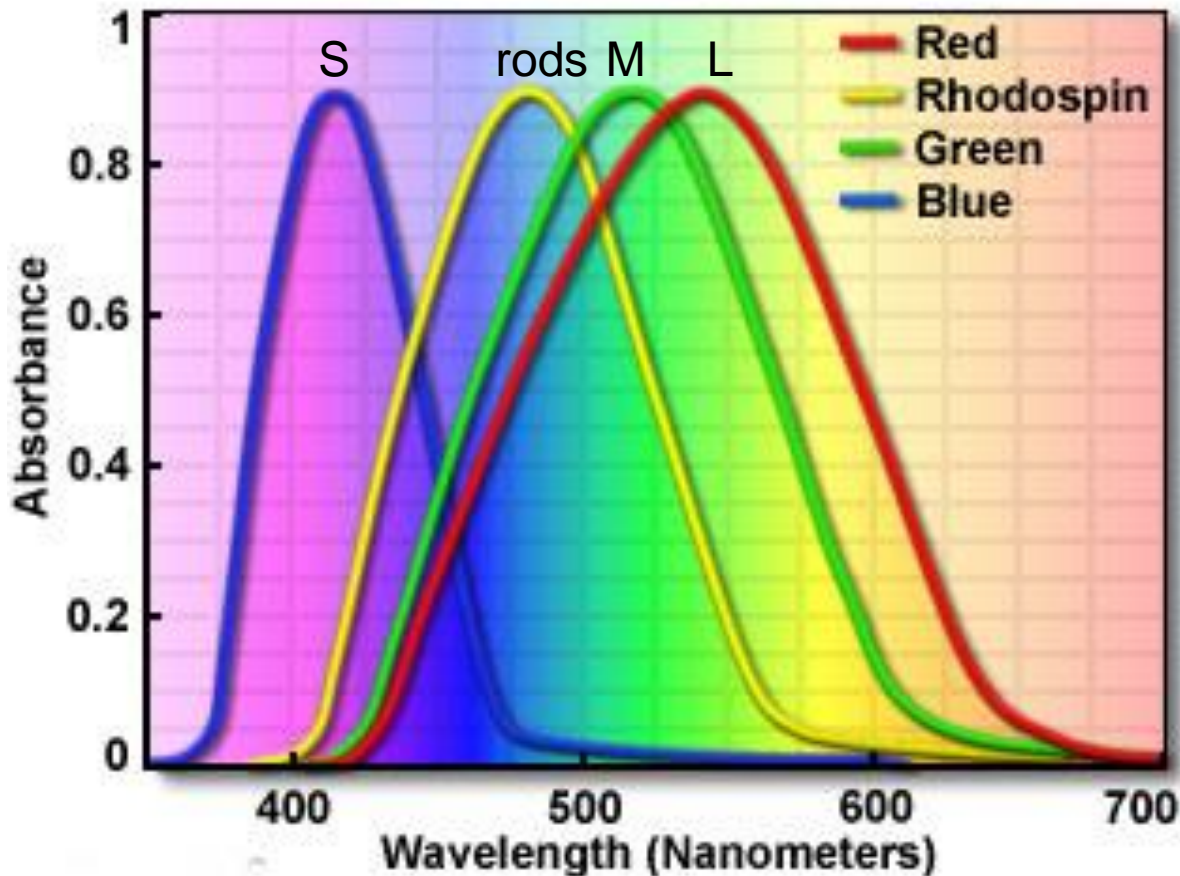
# Eye and retina



The retina is a **tri-dimensional** screen

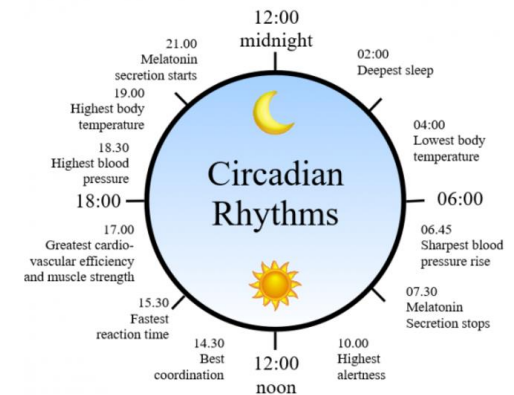
# Cones, rods, and ganglion cells

Absorption Spectra of Human Visual Pigments



- S-cones (420 nm) 5%
- M-cones (534 nm) 30%
- L-cones (564 nm) 65%
- Rods (498 nm)

ipRGC (555 nm)



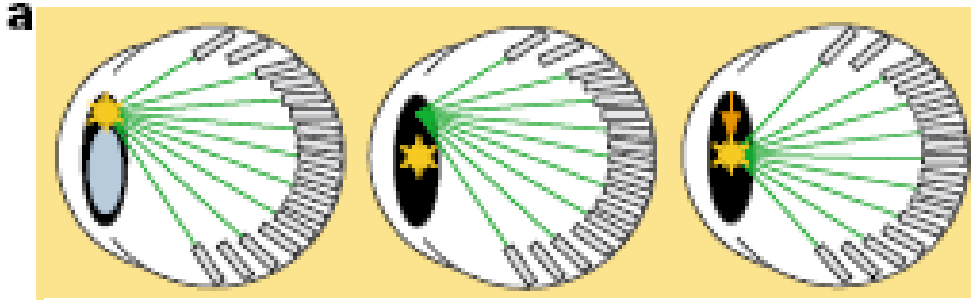
# Phototropism in plants



Sunflowers

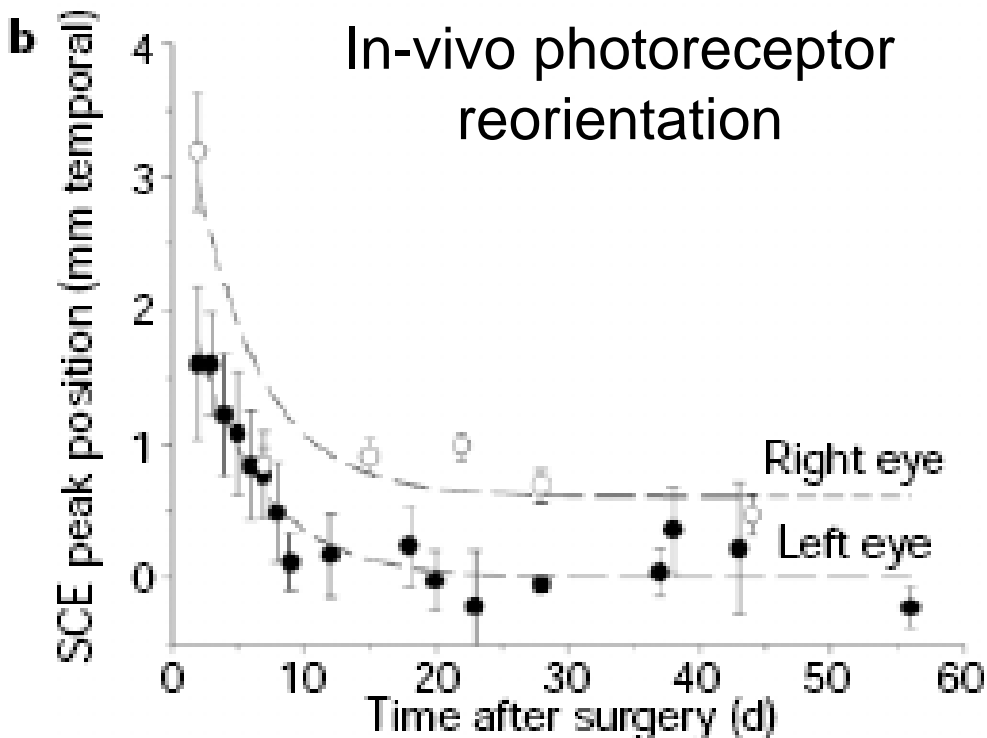
# Photoreceptors are likewise adaptable

Smallman et al., Nature **412** (2001) 604



Post-cataract surgery

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SCE peak displaced towards new pupil centre

Photoreceptors point to collect a maximum of light (phototropism)



# Outline

- **The Stiles-Crawford effect(s)**
- **Photoreceptor waveguides**
- **Geometrical optics model**
- **Electromagnetic models**
- **Myopia, emmetropization, and accommodation**
- **Directionality in diagnostic imaging**
- **Conclusions and outlook**

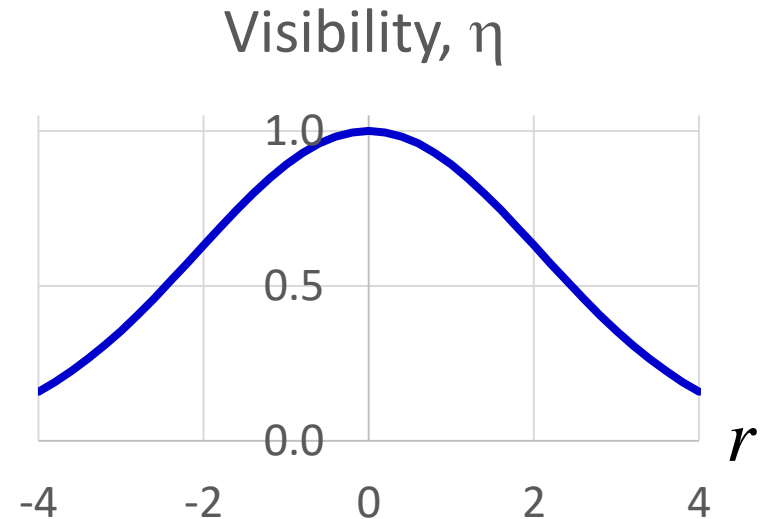
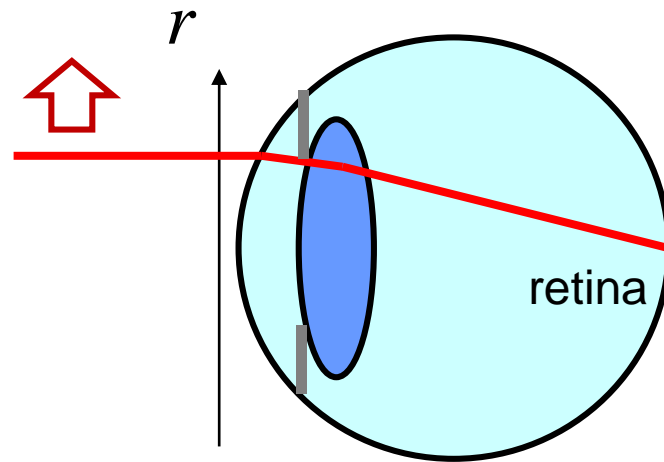
# Directionality with Maxwellian light

## The Stiles-Crawford effect (SCE-I)

Proc. Roy. Soc. 1933



Walter S. Stiles



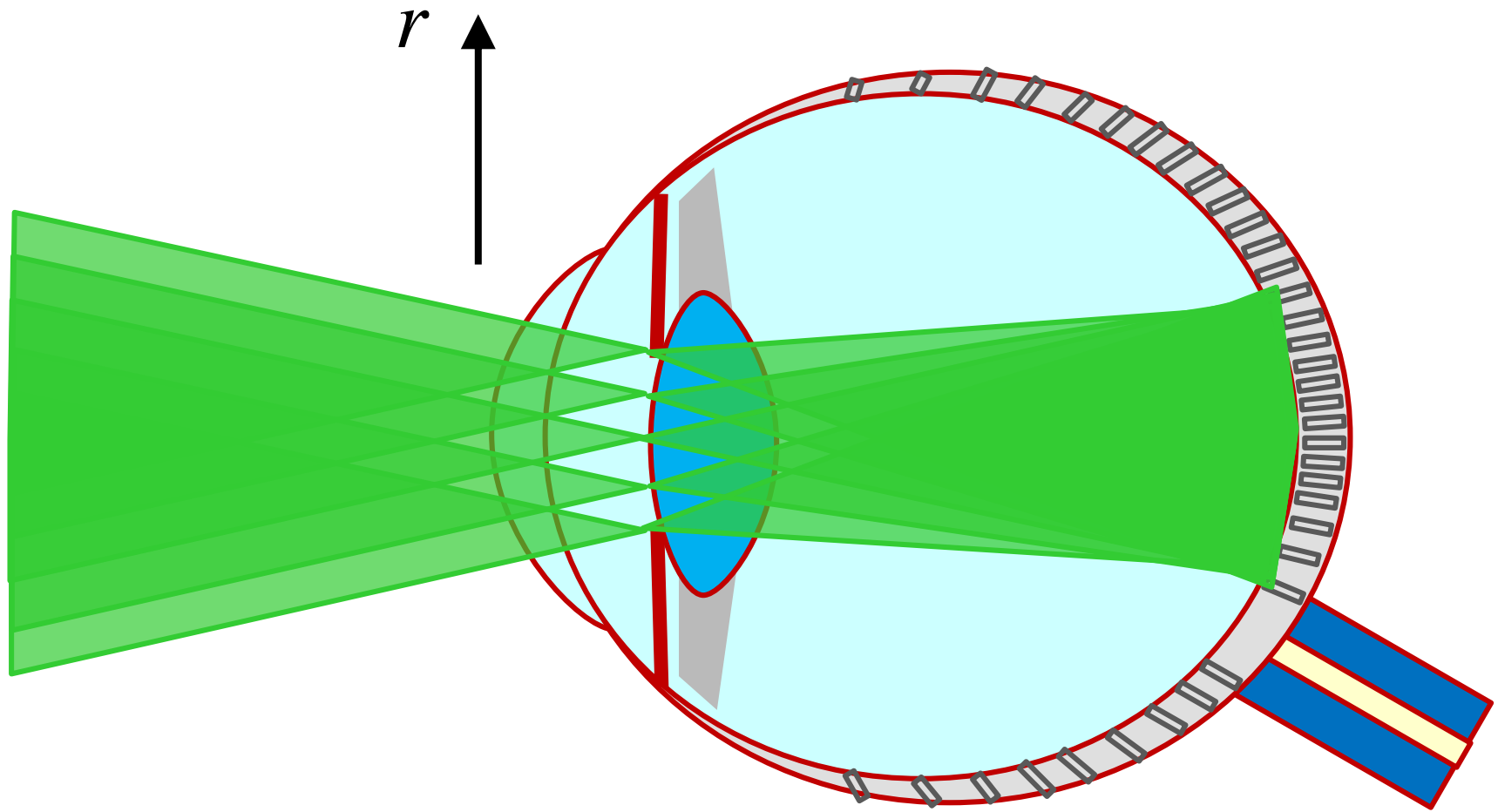
Visibility for oblique rays:

$$\eta(r) = \eta_{\max}(r_{\max}) 10^{-\rho_{SCE} |r - r_{\max}|^2}$$

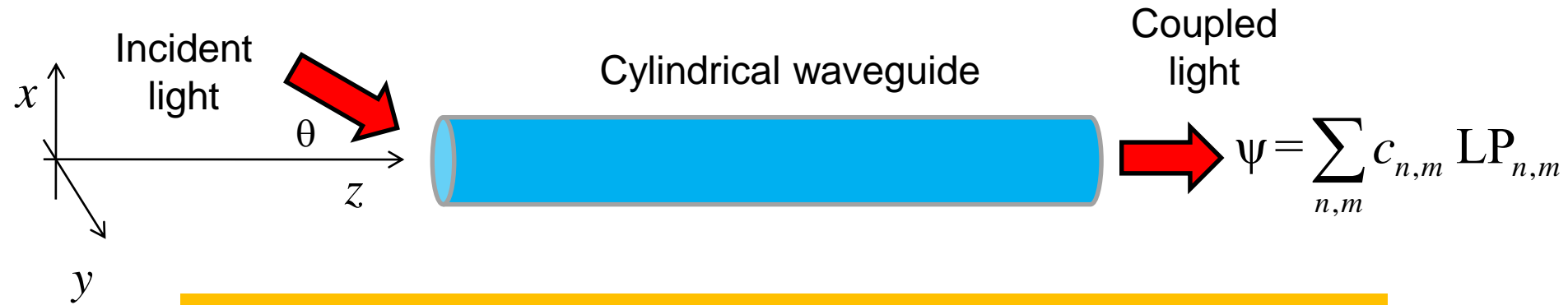
Brian H. Crawford

Foveal directionality parameter  $\rho_{SCE} \cong 0.05/\text{mm}^2$

# Maxwellian light

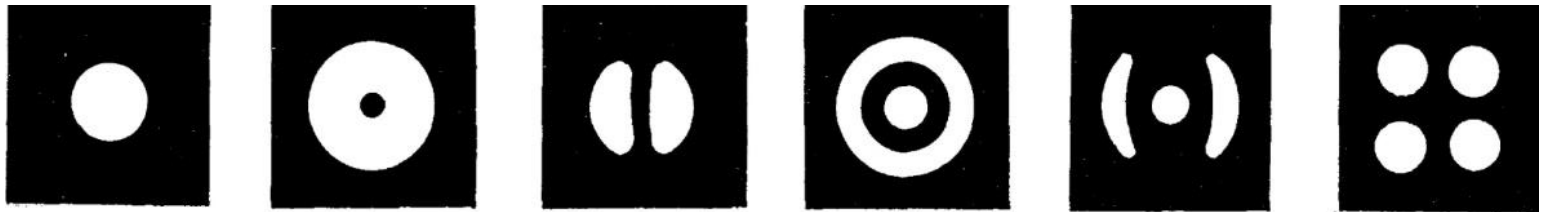


# Real-eye cone-photoreceptor waveguides



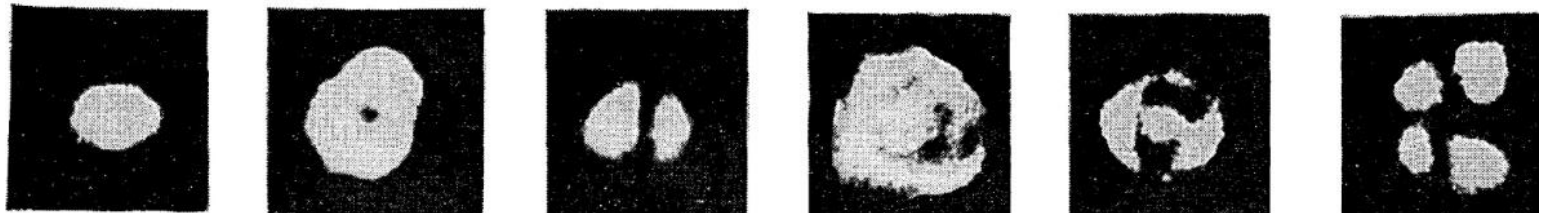
- Fovea cones: single (or few) mode waveguides
- Parafovea cones: low-order multimode waveguides

Model



Cutoff  $V=3.8317$

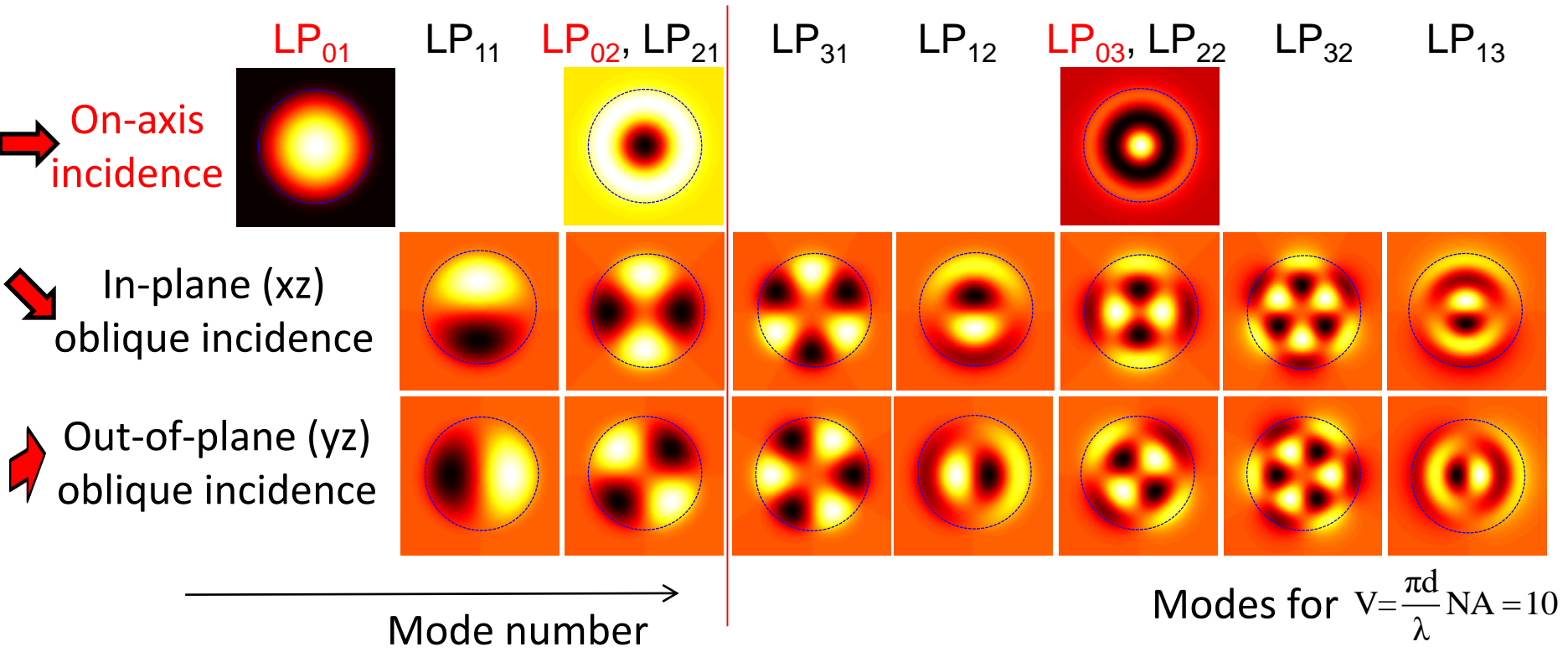
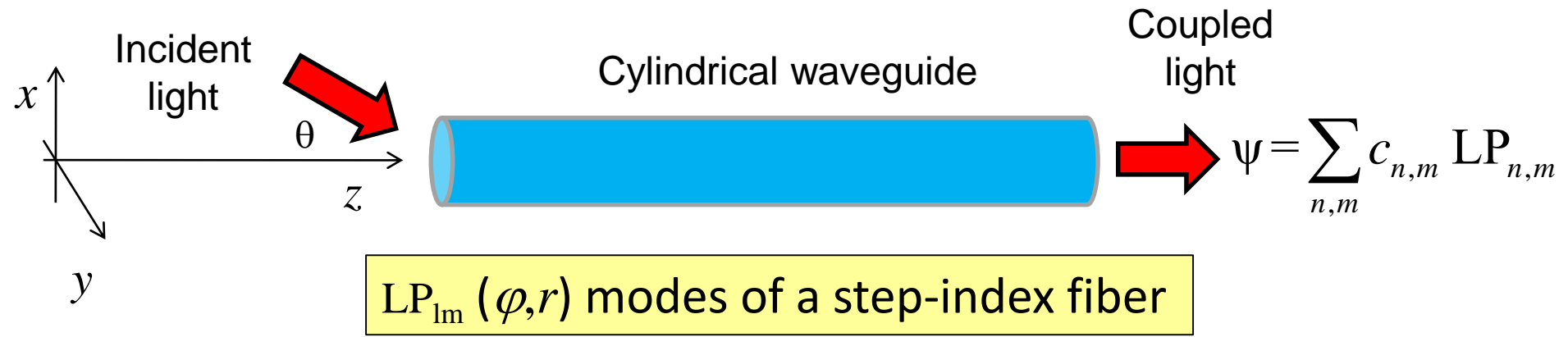
Experiment



Outer segment modes of **rat, monkey, and human** (Enoch, JOSA 1963)

Mode number

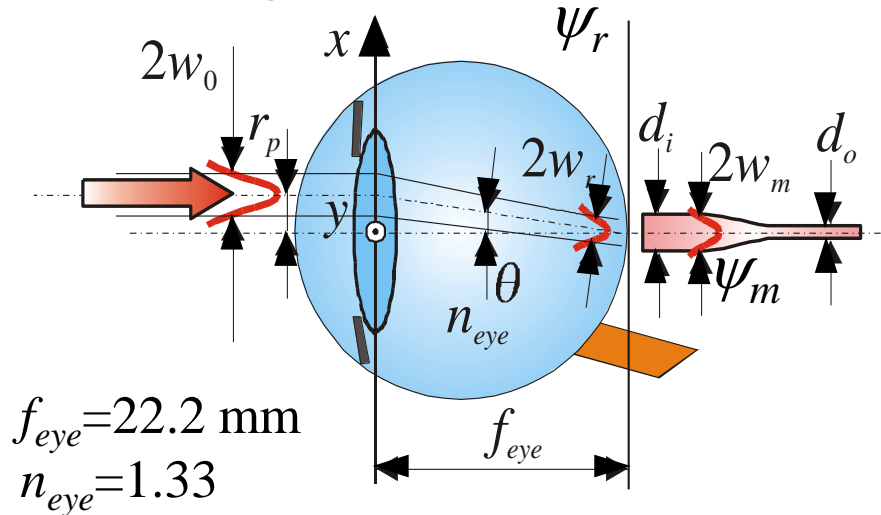
# Cylindrical waveguide photoreceptor model



# Light coupling to a Gaussian mode

Vohnsen *et al*, JOSA A **22** (2005) 2318

Shifting of a narrow incident beam



SCE-I function at the pupil

$$\eta(r) = \eta_{\max} 10^{-\rho_{SCE} (r - r_{\max})^2}$$

Directionality factor

Single waveguide derivation of  $\rho_{SCE}$

Coupling strength:

$$T = \left| \iint \psi_r \psi_m^* dudv \right|^2$$

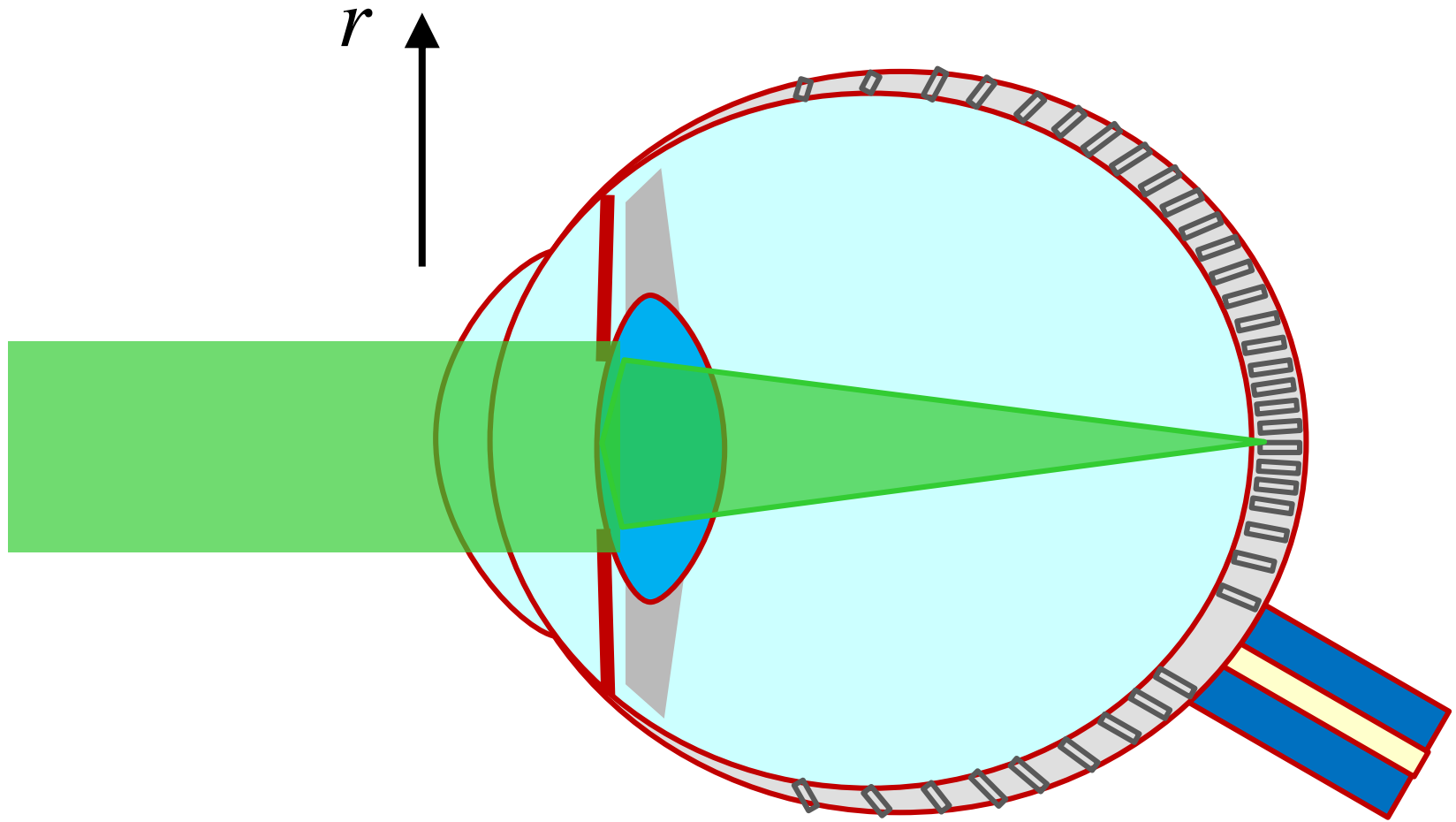
Gaussian beam and mode approximation (matched  $w_m = w_r = w$ )

SCE-I directionality factor

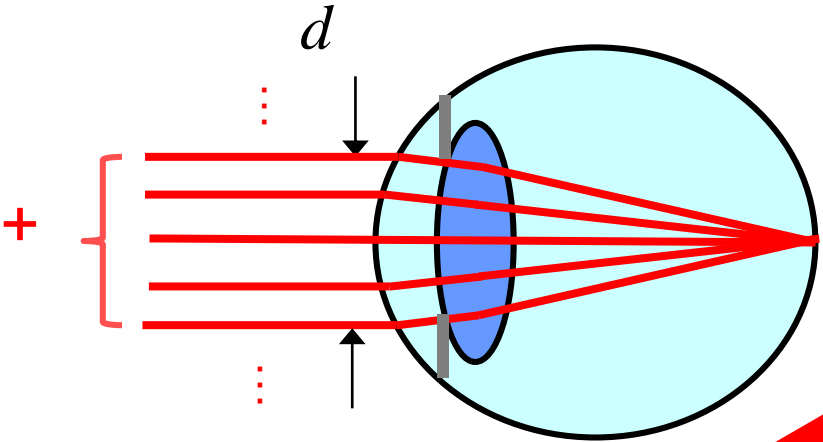
$$T(\theta) = \exp \left[ - \left( \frac{\pi n_{eye} w}{\lambda} \right)^2 \theta^2 \right]$$

$$\rho_{SCE} = \log(e) \left( \frac{\pi n_{eye} w}{\lambda f_{eye}} \right)^2$$

# Normal vision (Newtonian light)

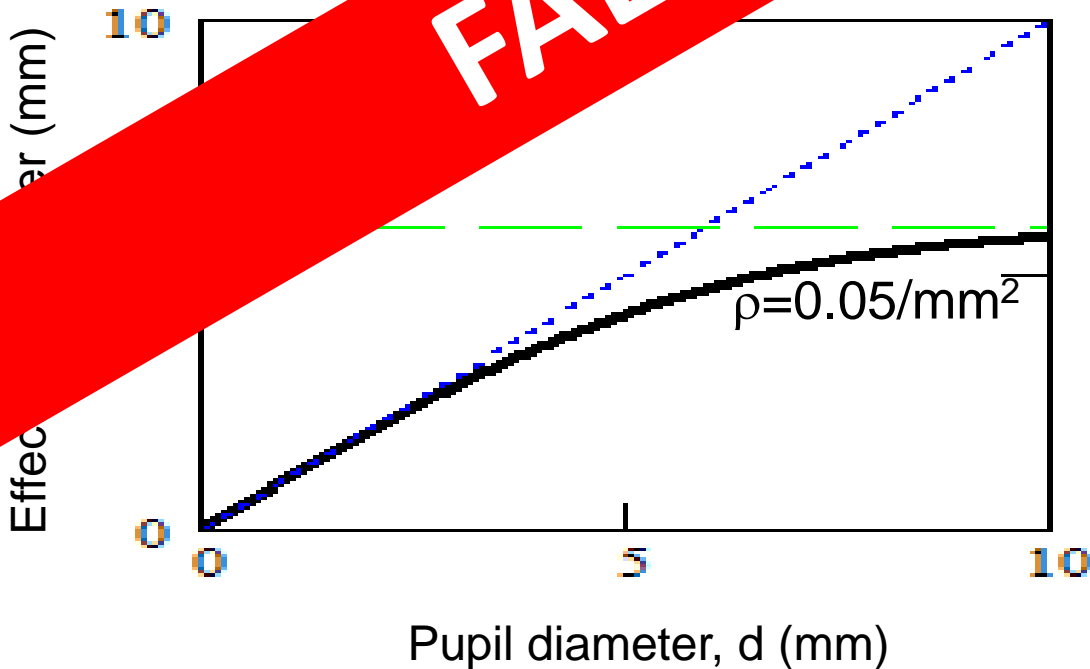


# Integrated SCE (normal vision)



Integrated SCE for a pupil

$$\eta_{eff}(d) = \int_0^d \rho_{SCE} r^2 r dr$$



True or false?



**What **are** the Stiles-  
Crawford effects**s**?**

# Psychophysical:

**SCE-I**

**SCE-II**

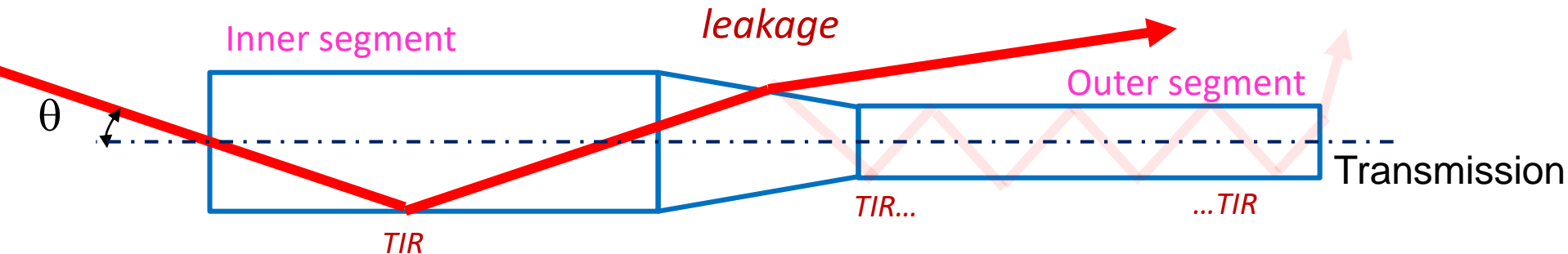
**INTEGRATED SCE-I**

# Objective:

**OSCE**

# What *is* the SCE-I?

## Geometrical-optics interpretation



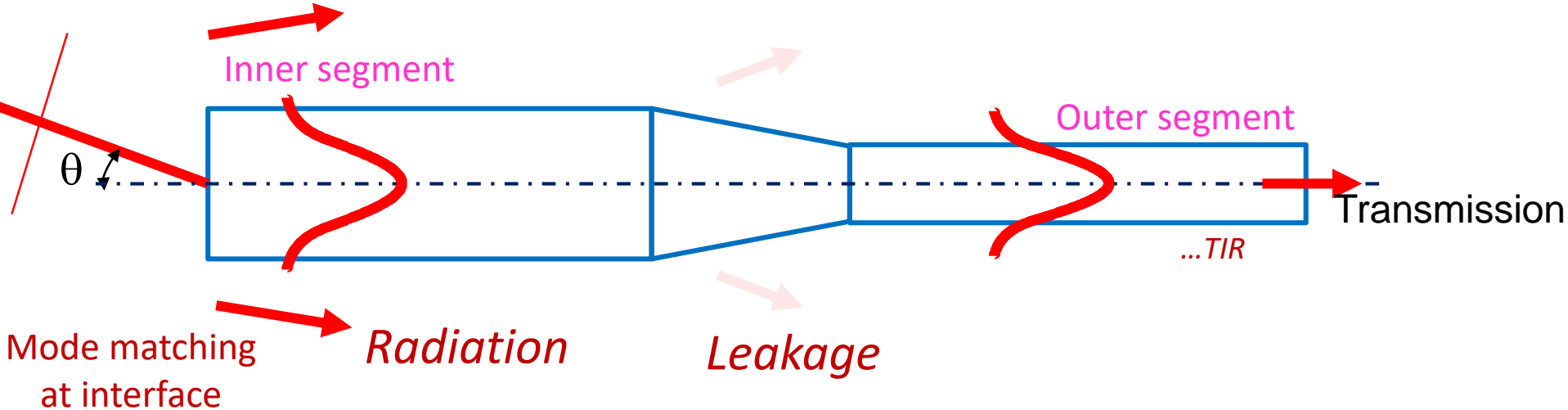
- ❑ Leakage of rays above a critical angle (O'Brien, JOSA 1951)
- ❑ Disarray of neighbouring photoreceptors (Safir & Hyams, JOSA 1969)

### Problems?

- “Sharp” cut-off above a certain angle of incidence
- This is transmitted light, not absorbed (vision) light
- How can it describe cylindrical foveal cones? ... or rods?

# What *is* the SCE-I?

## Wave-optics interpretation



- Fibre-optical waveguide modes (Snyder & Pask, Vis. Res. 1973)
- Gaussian mode coupling (Vohnsen, Iglesias & Artal, JOSA A 2005)

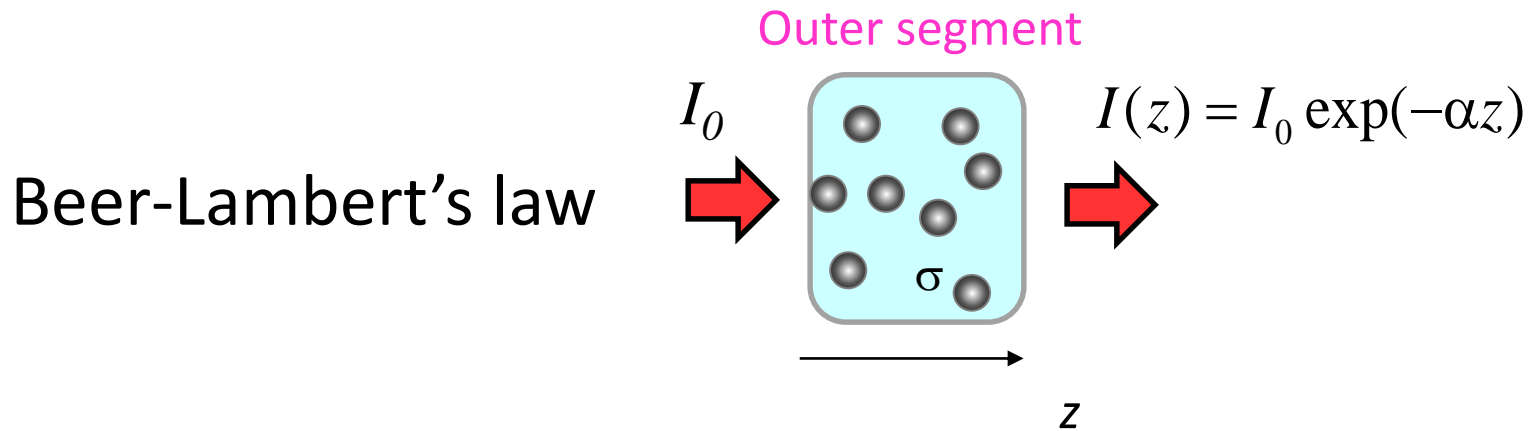
## Problems?

- What happens to the nonguided radiative modes?
- This is transmitted light, not absorbed (vision) light
- How can it describe densely-packed waveguides?

**Where is vision  
triggered?**

# Geometrical-optics solution

We need to consider light *absorption*

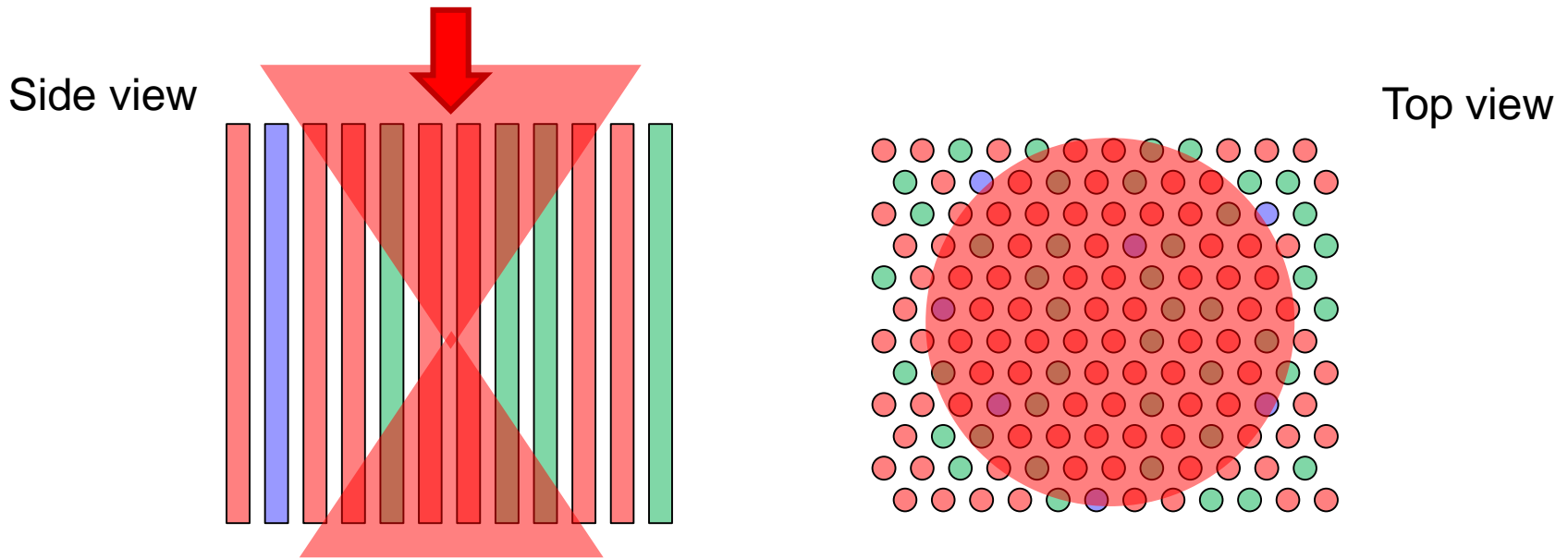


Visibility (absorption) is proportional to distance (1<sup>st</sup> order)

$$\eta = 1 - \exp(-\alpha z) \cong \alpha z$$

In 3-D this is a “volumetric” absorption model

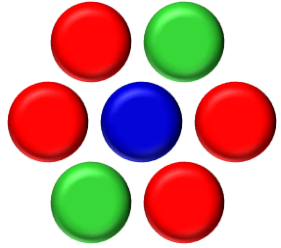
# Visibility: light-pigment overlap



$$\eta = \frac{\text{intersection volume}}{\text{light volume}} \leq 1$$

Volumetric overlap gives an estimate for the absorption and visibility

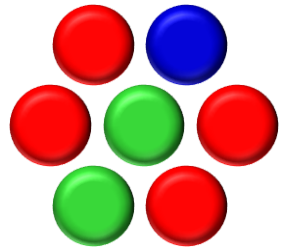
# Example for the SCE-II



S-cones surrounded by mostly M and L

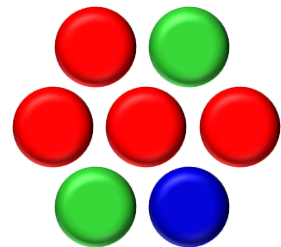
Hue shift

$$\Delta\lambda > 0$$



M-cones surrounded by L, M and some S

$$\Delta\lambda \cong 0$$

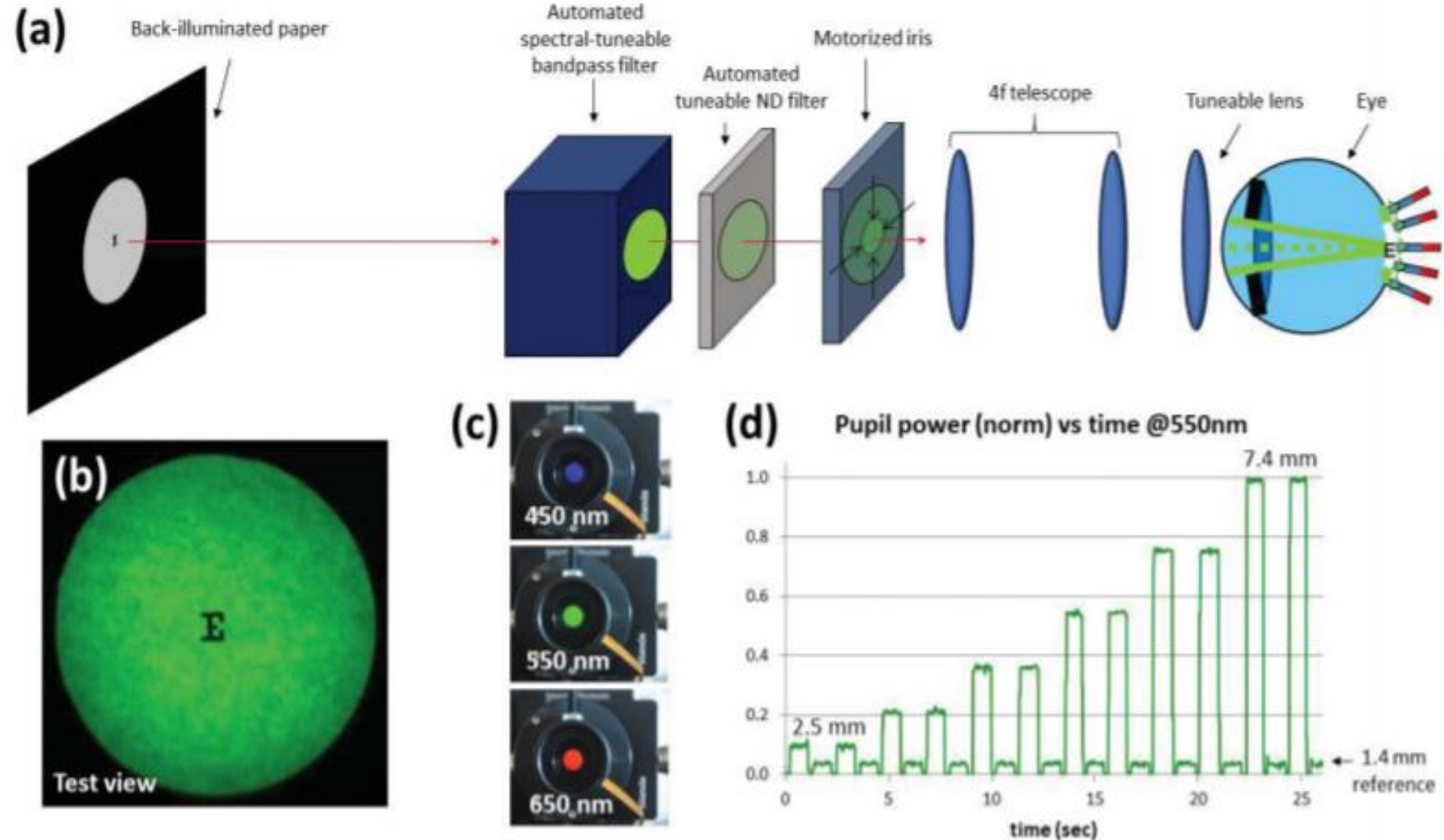


L-cones surrounded by L, M and some S

$$\Delta\lambda < 0$$

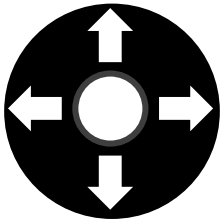


# Integrated SCE-I measurements

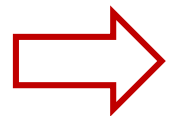


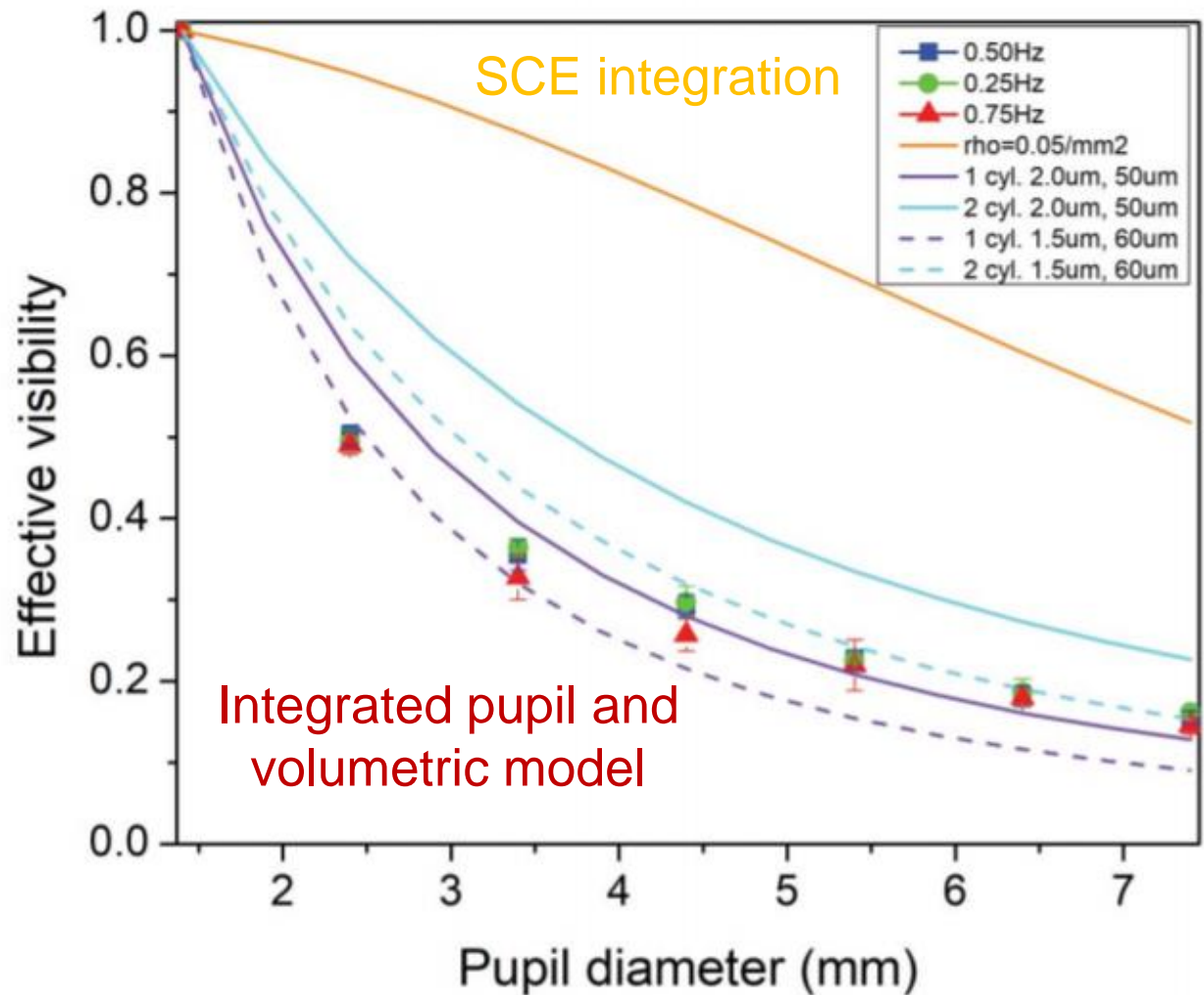
# Integrated SCE-I: pupil size flickering

Experimental verification  
of the volumetric  
absorption model



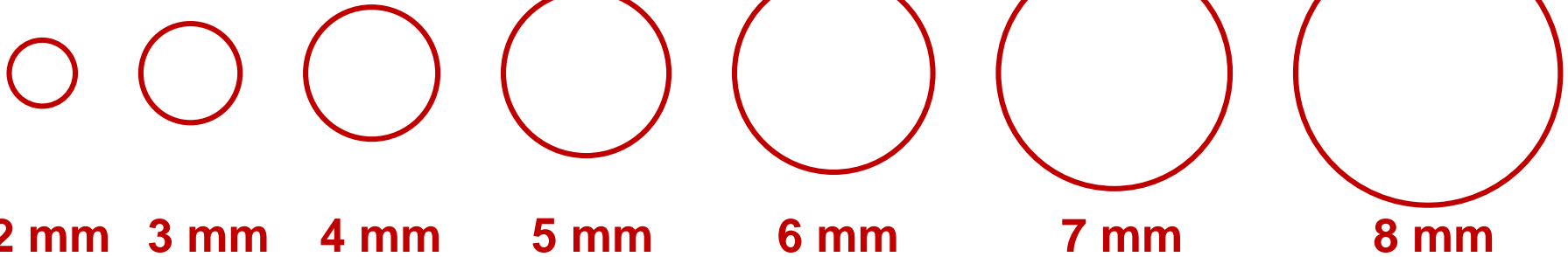
A small pupil is most effective

  $\rho \cong 0.40/\text{mm}^2$

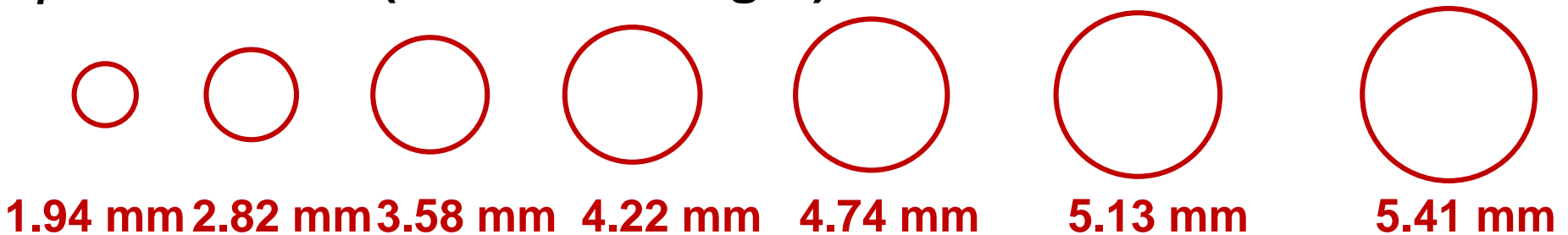


# Effective pupil

No SCE-I



$\rho = 0.05/\text{mm}^2$  (Maxwellian light)

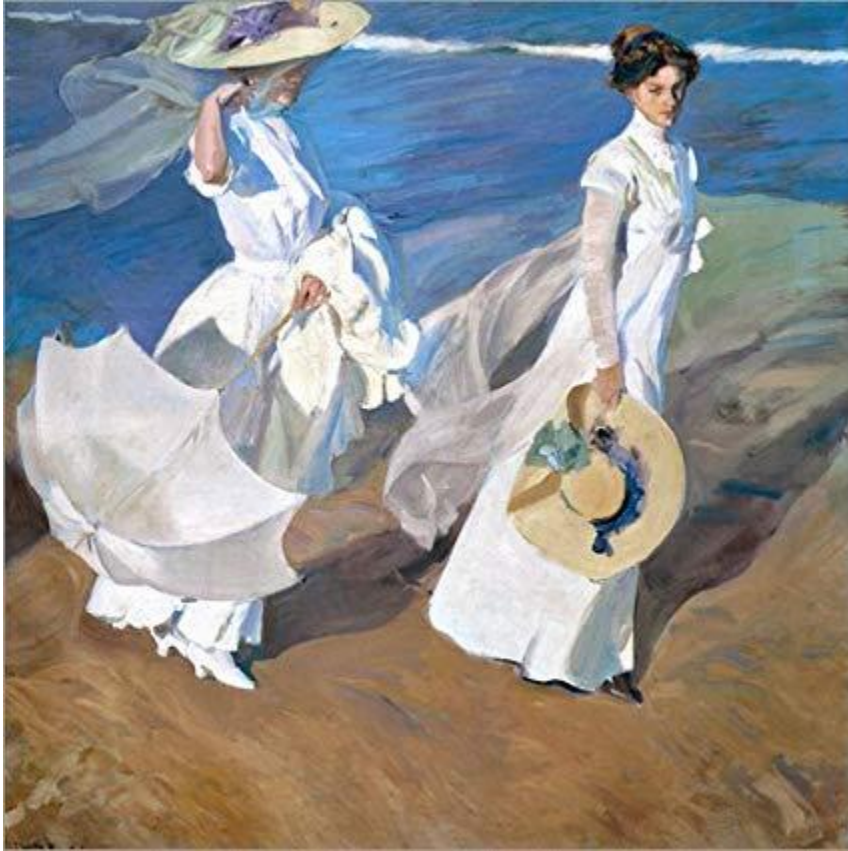


$\rho = 0.40/\text{mm}^2$  (Normal vision)



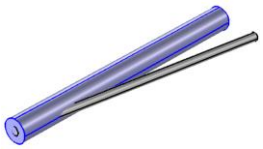
# Integrated SCE-I and reduced MTF quality

Vision @ 2 mm pupil

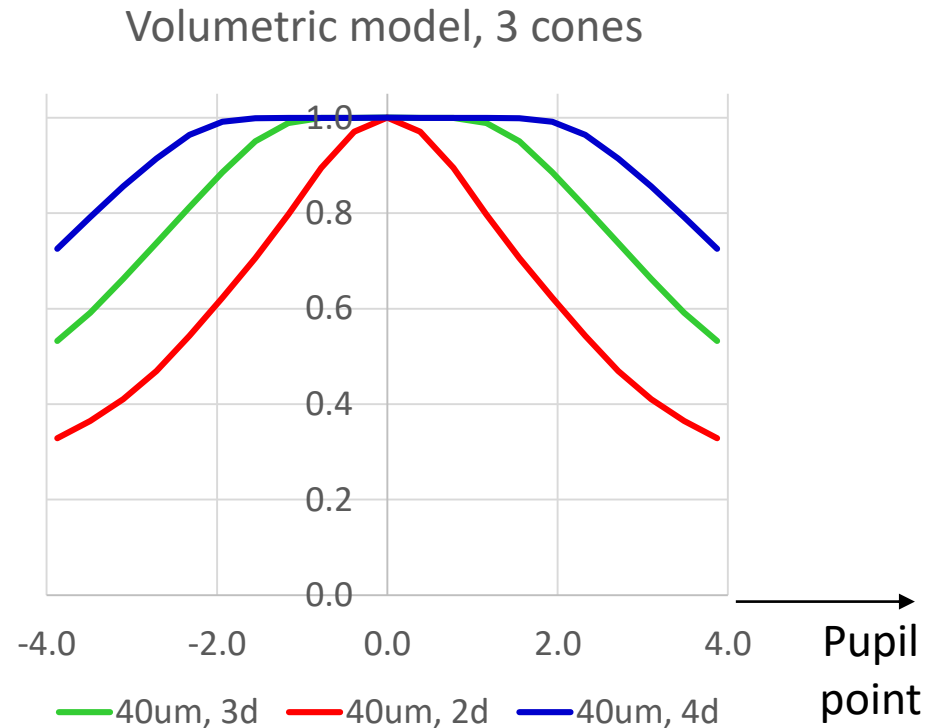
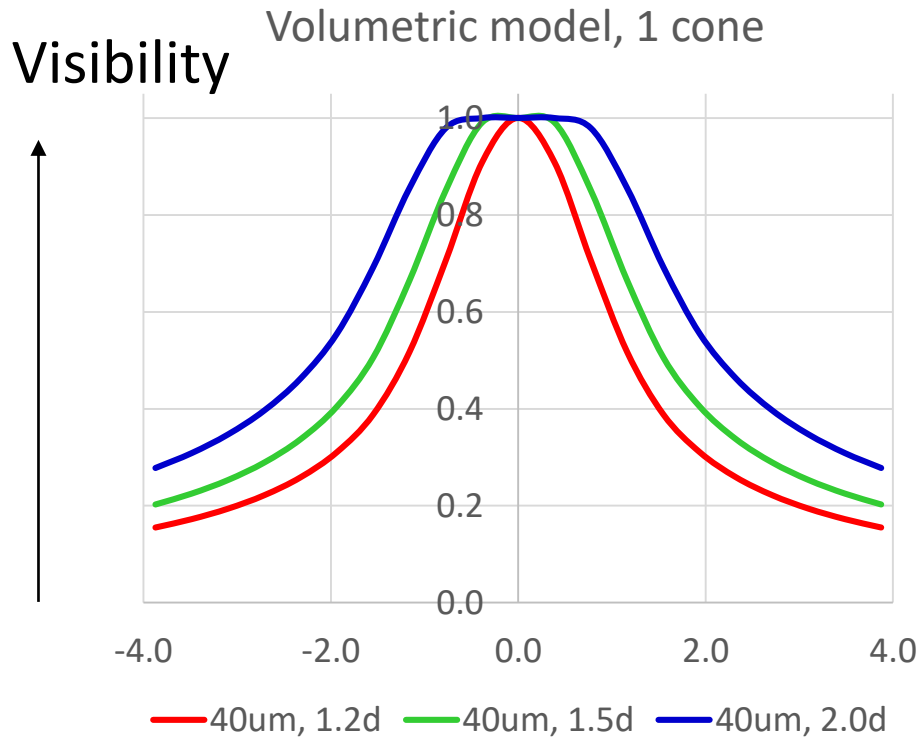
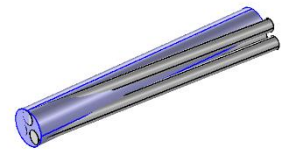


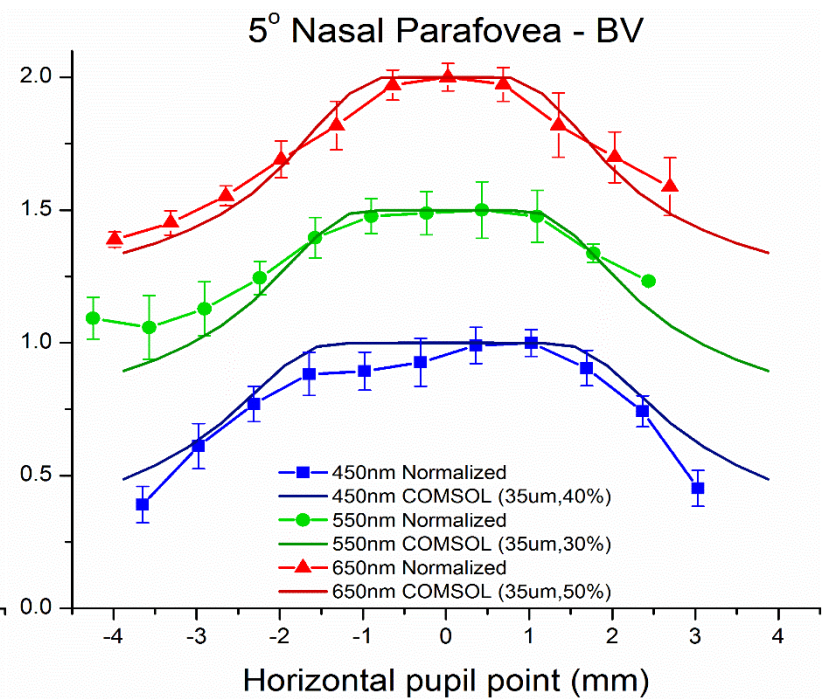
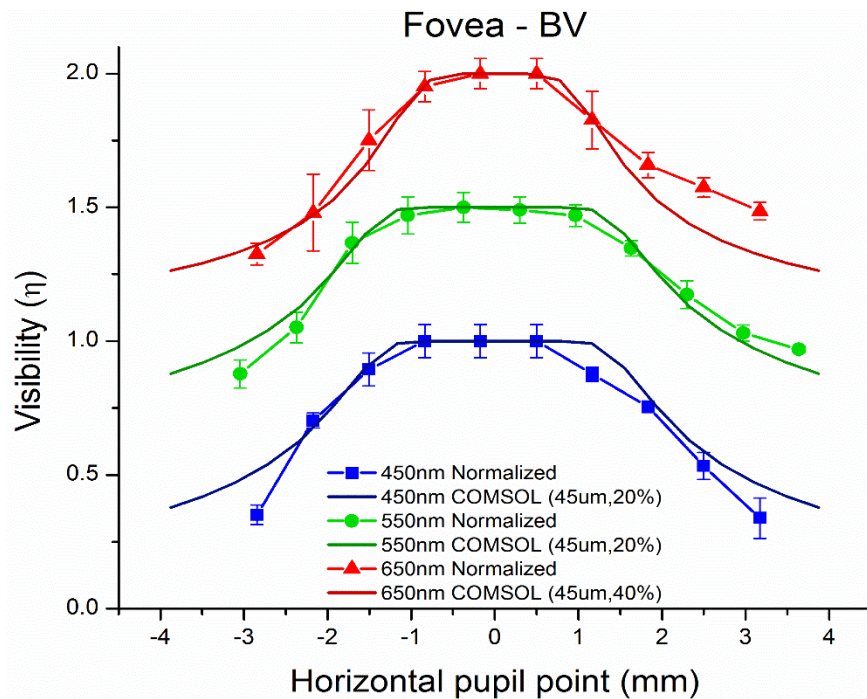
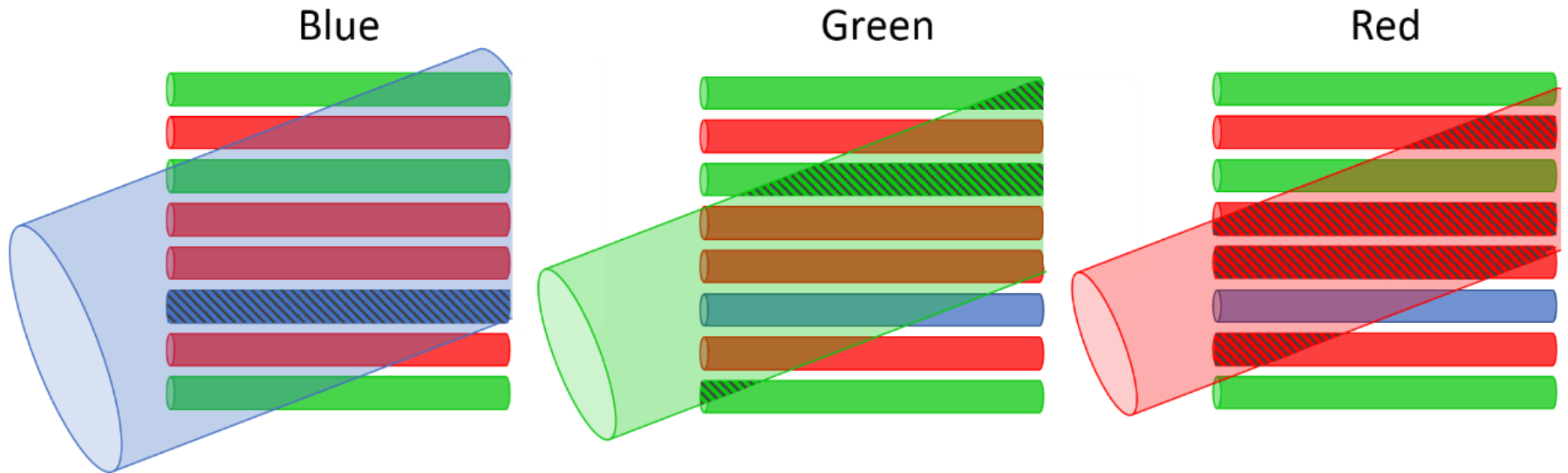
Vision with retinal blur @ 8 mm pupil





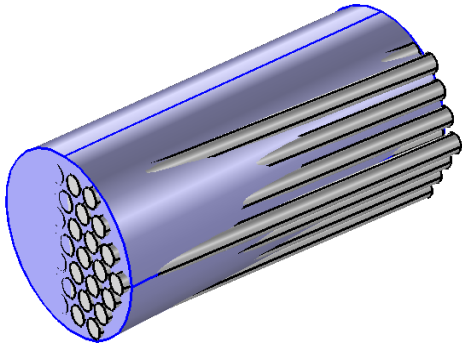
# Examples for the SCE-I



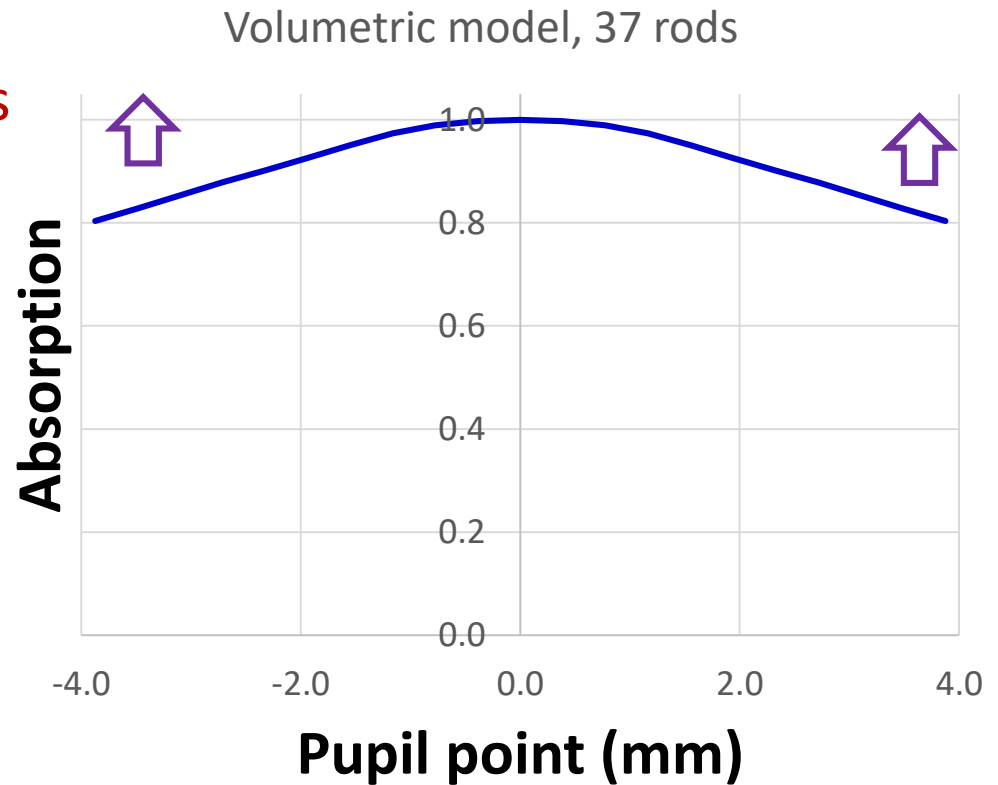


# Why do rods lack directionality?

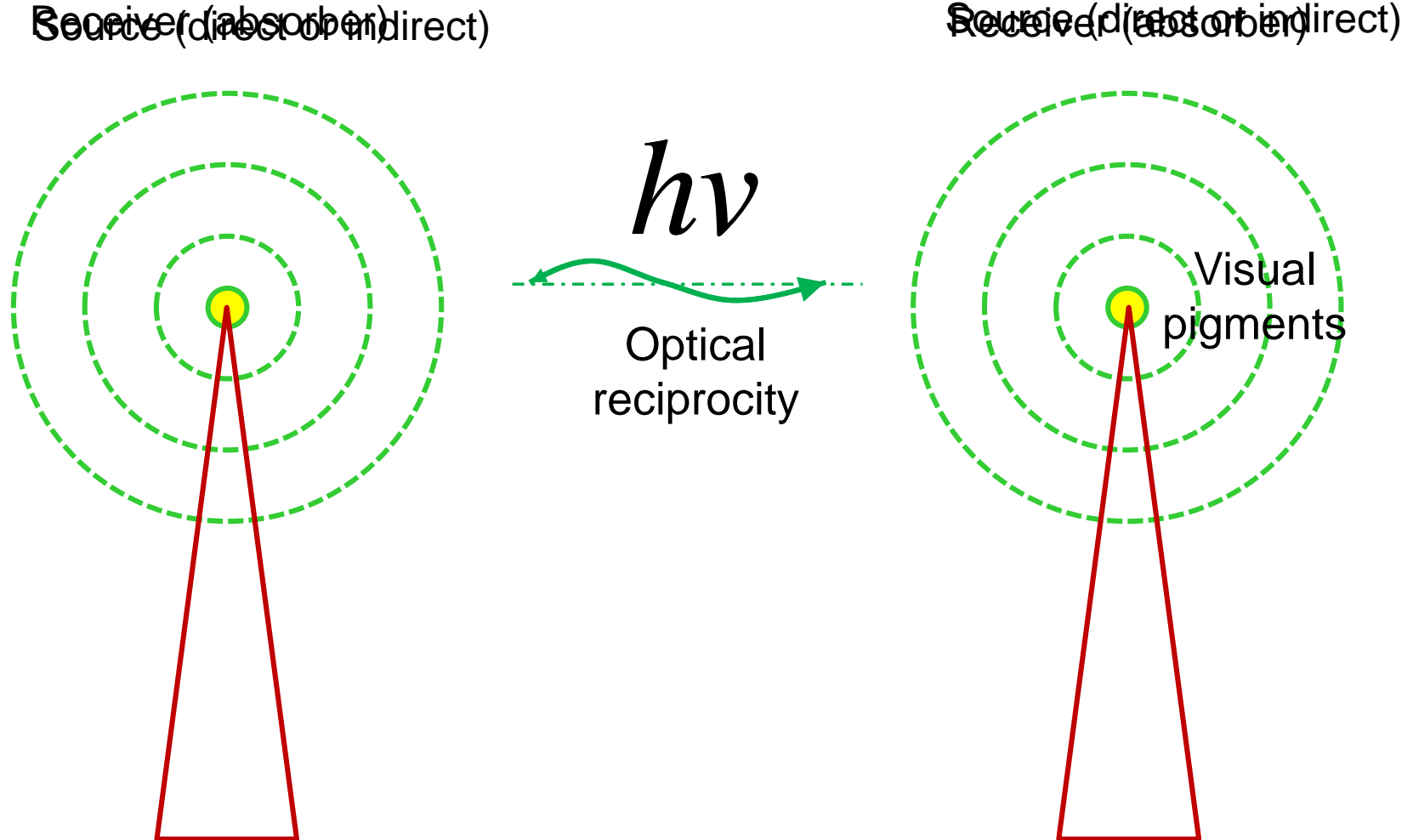
Rods are surrounded by ... rods



$$\rho_{SCE} \cong 0$$



# Antenna model



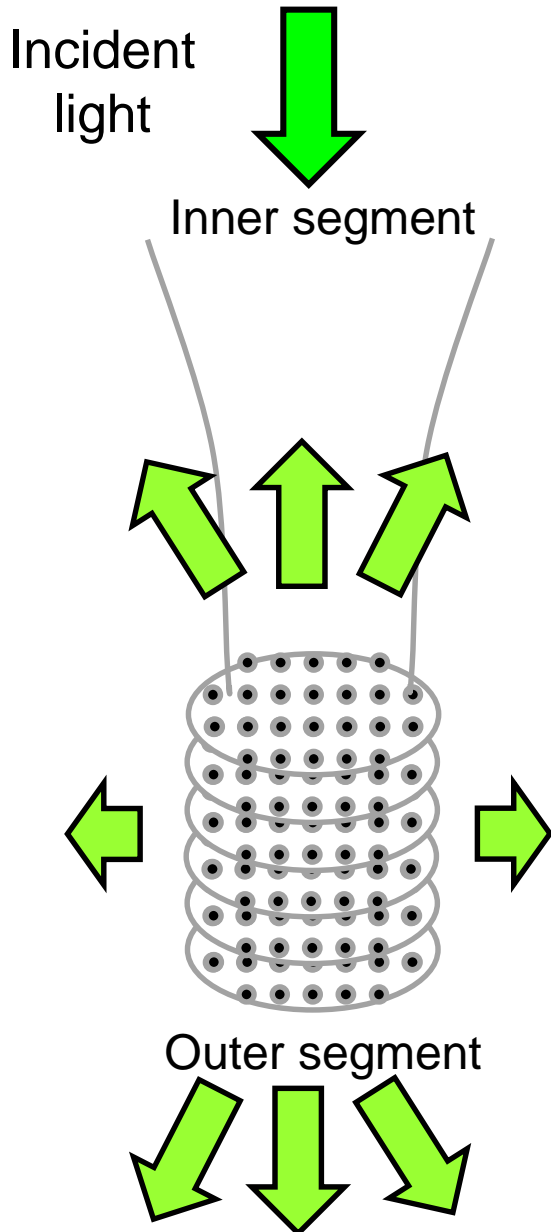


# Outer segment membrane stacking and visual pigments



Modelo de tortillas

# Dipolar antenna model of outer-segment pigments



## Model data:

Pigments can be considered as dipole antennas ( $\varnothing 5$  nm)

Each disc has from 4,000 ( $\varnothing 1$   $\mu\text{m}$ ) to 4,000,000 ( $\varnothing 5$   $\mu\text{m}$ )\*

Each outer segment has approximately 1000 lamellae\*

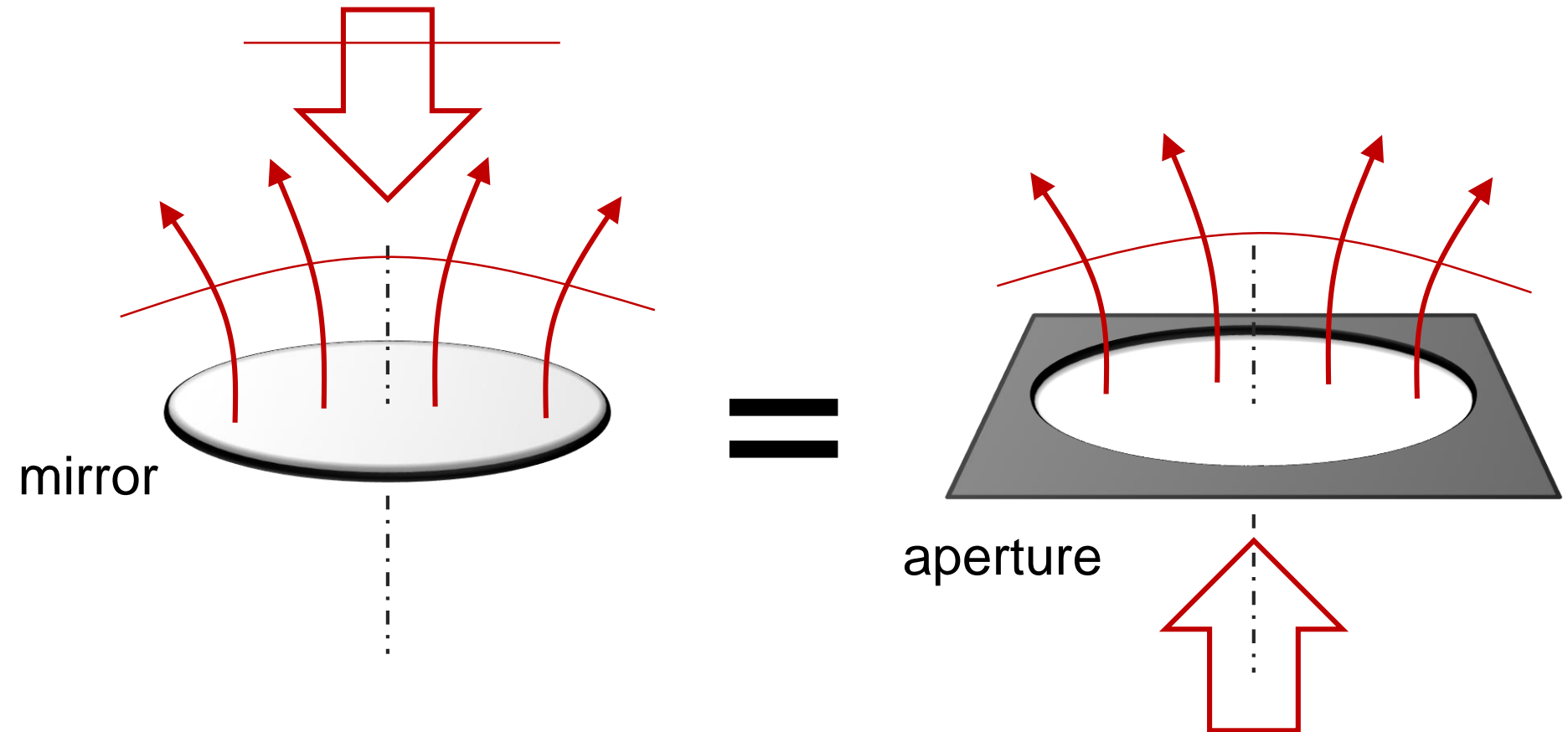
Lamellae interspacing is approximately 20 nm\*

Membrane wall thickness (5 nm) is ignored

Dipoles are assumed to be uncoupled

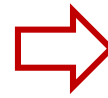
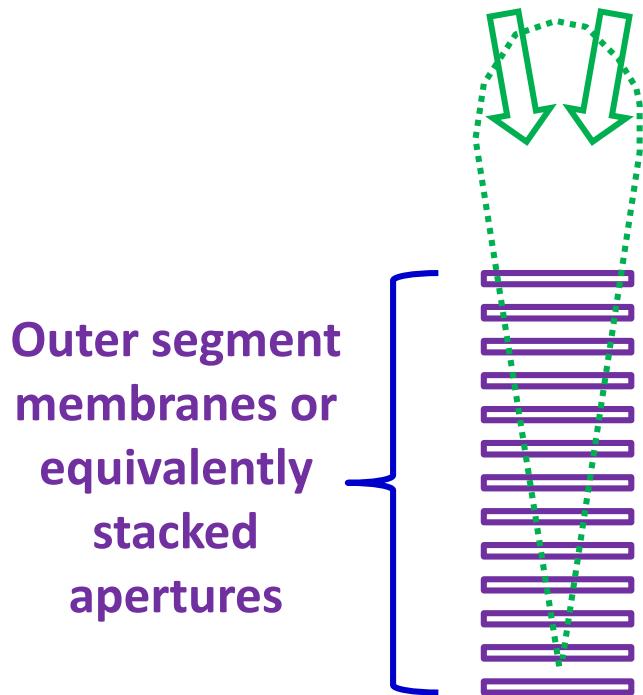
\* J. J. Wolken, "Light detectors, photoreceptors, and imaging systems in nature" (Oxford, 1995)

# Diffraction equivalence (1 disc)

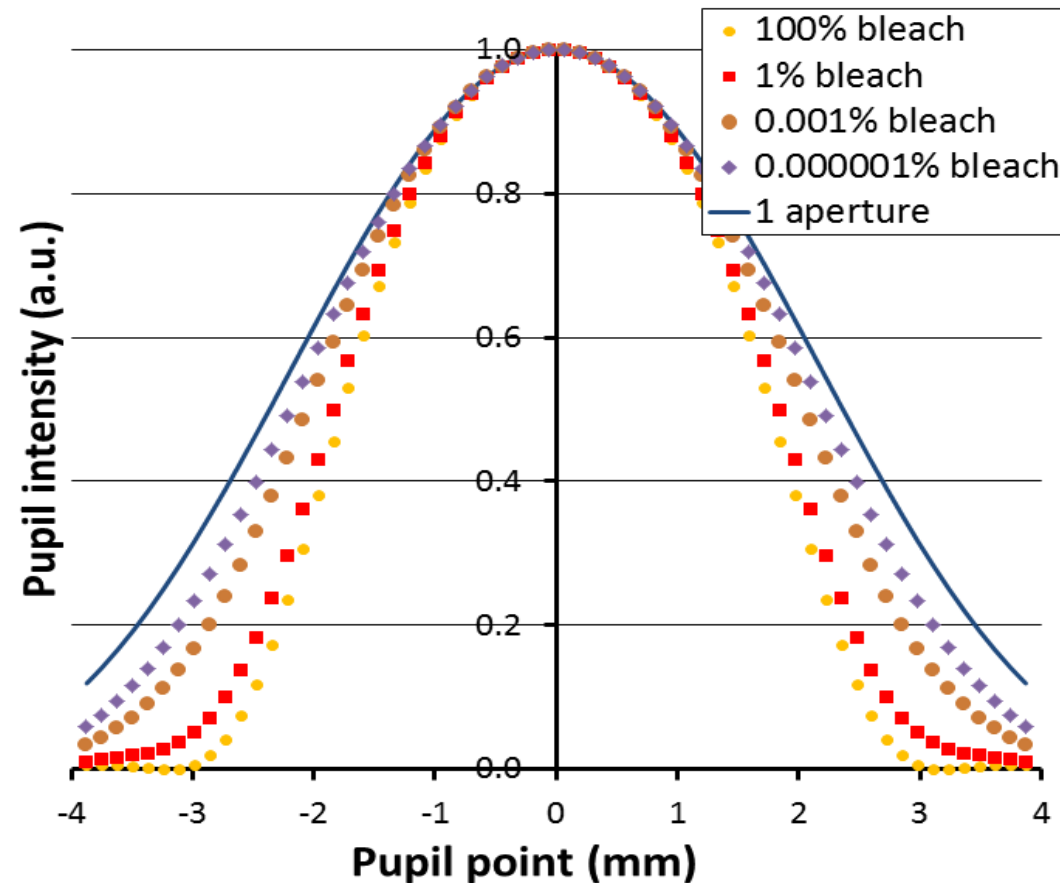


# Electromagnetic *scattering* model

## Multilayer antenna model and optical reciprocity



$\rho$  in the range of 0.05 (dim light) –  
0.10 /mm<sup>2</sup> (bleached)



# Oblique incidence on one outer segment

740 molecules  $\times$  1000 discs

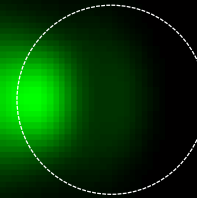
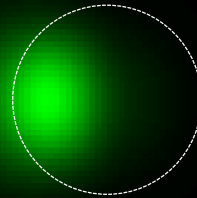
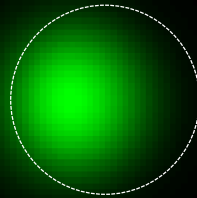
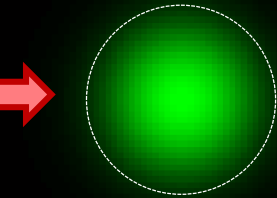
Total scattered field vs. incidence angle:

0 deg.

5 deg.

10 deg.

15 deg.



20  $\mu\text{m}$

For oblique incidence, scattered light shifts to one side of the segment.  
With a conical outer segment (not shown) the axial light becomes more confined

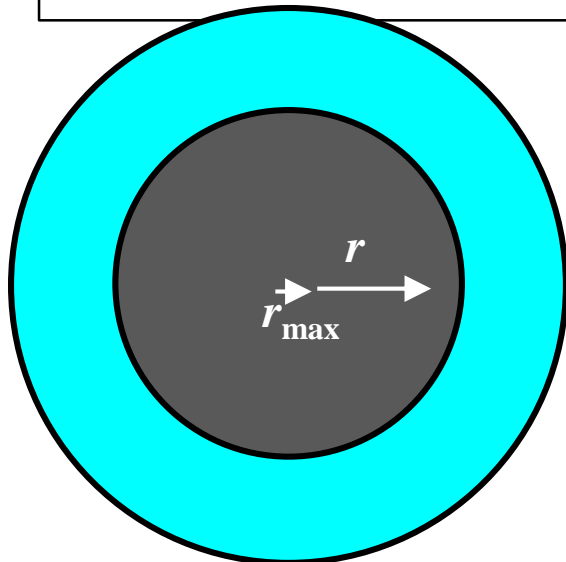
# A “new” Stiles-Crawford fitting function

Airy-disc pupil function for relative visibility/intensity:

$$\eta(r) = \eta_{\max}(r_{\max}) \left[ 2 \frac{J_1(\alpha |r - r_0|)}{\alpha |r - r_0|} \right]^2$$

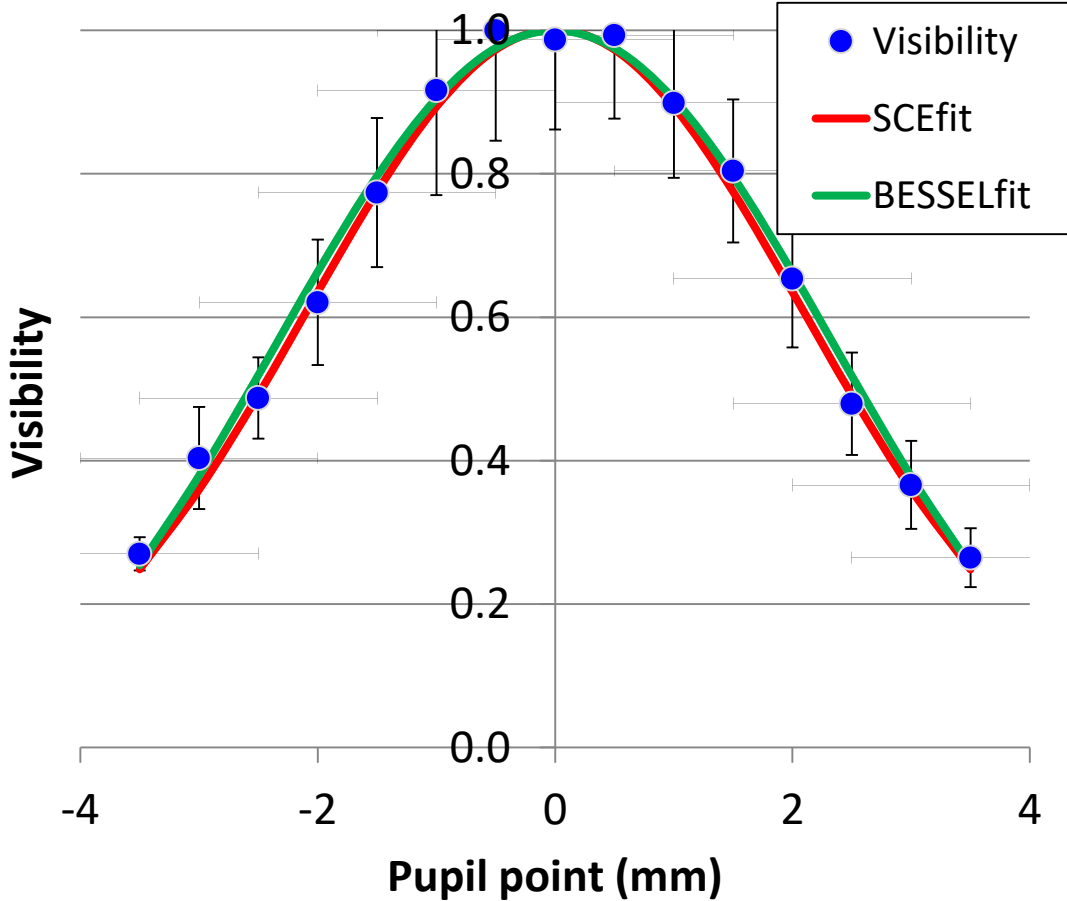
Peak of visibility  
(or intensity)

New directionality  
parameter



# Gaussian vs. Airy SCE-I function

Subject BV 550nm (experiment)  
12 measurement-series averaged



Gaussian SCE function?

$$\eta(r) = 10^{-\rho(r-r_0)^2}$$



or Airy disc function?

$$\eta(r) = \left[ 2 \frac{J_1(\alpha(r-r_0))}{\alpha(r-r_0)} \right]^2$$

# Increased myopia prevalence

Excessive eye growth affecting 50% of the world population by 2050

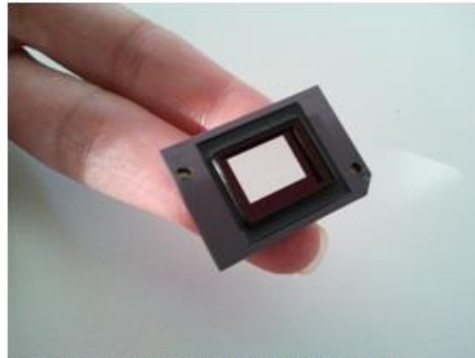
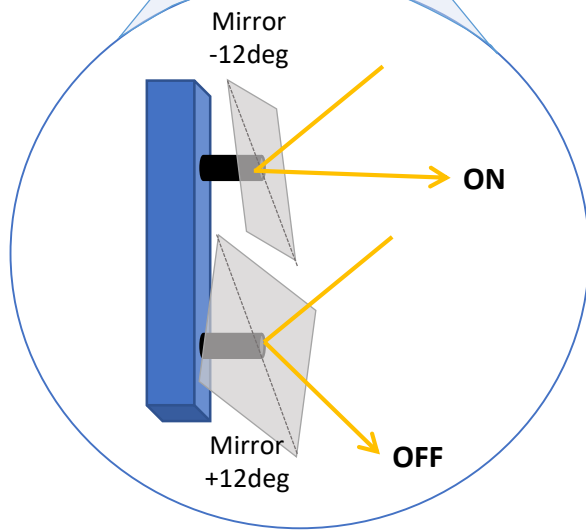
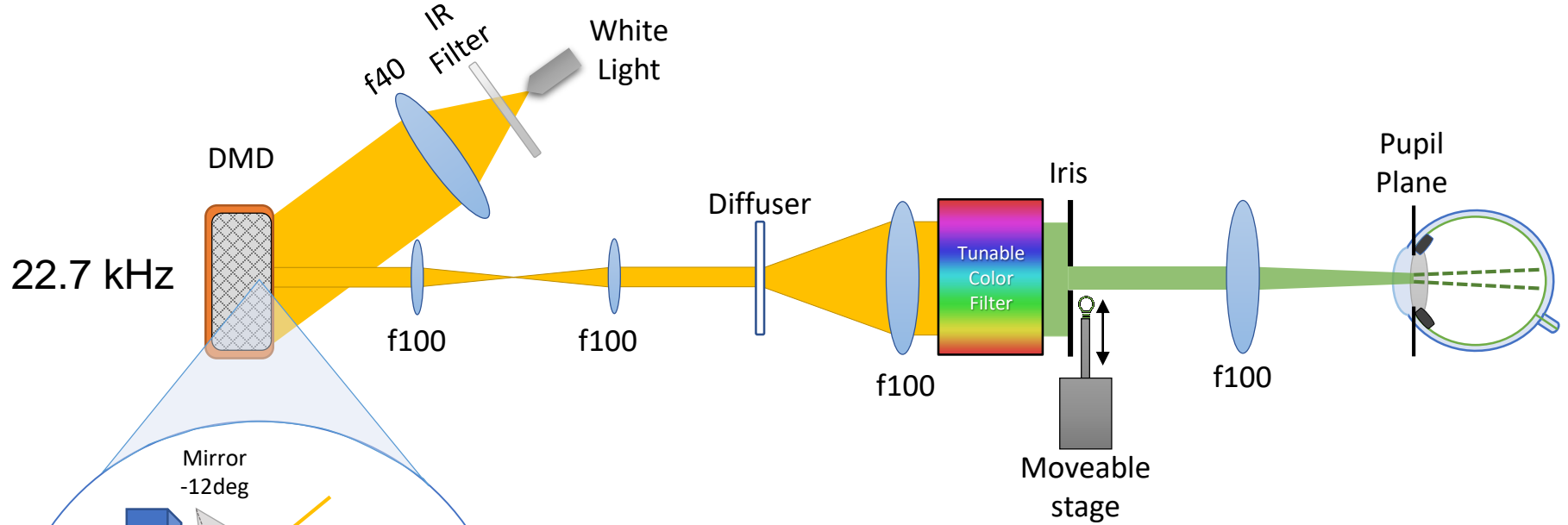


Increased risk of  
retinal detachment  
and glaucoma

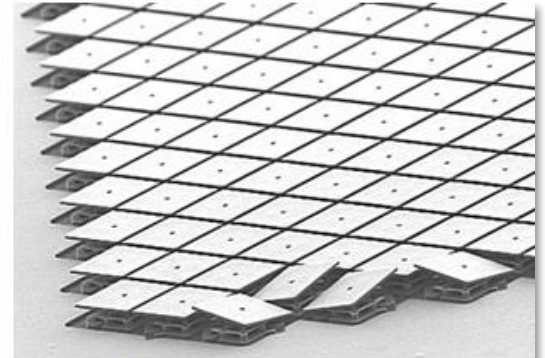
“The myopia boom” Nature (2015)



# SCE-I analysed in myopes, uniaxial system

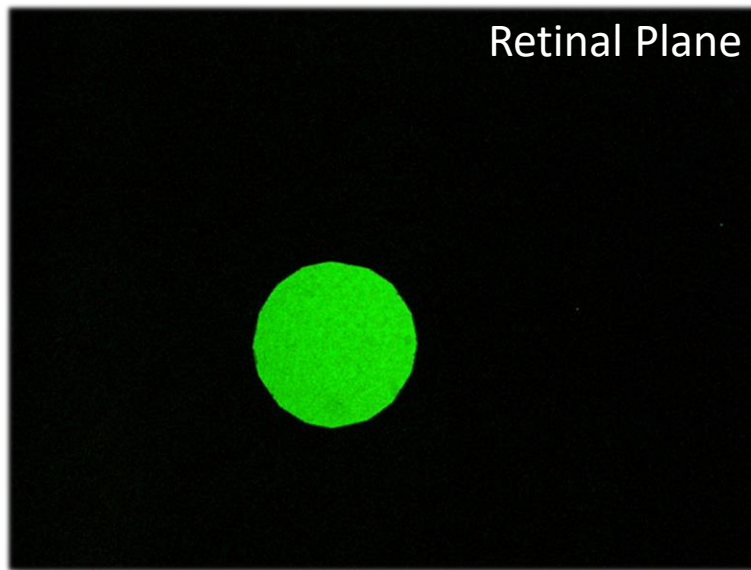


DIGITAL MICRO MIRROR DEVICE (DMD)  
(SLM - Spatial Light Modulator)



MICRO MIRRORS CLOSE UP

# Uniaxial brightness flicker



**INPUTS**

Period (ms)

0.044 30

26.999

37.0384 Hz

**Reference**

REF Duration (ms)

1000

1 Hz

REF On-Time (ms)

0.044 30

6.605

151.4 Hz

**Scanning Image**

IMG Duration

1000

1 Hz

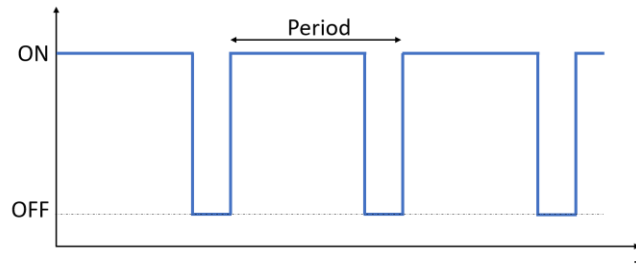
IMG ON-Time (ms)

0.044 30

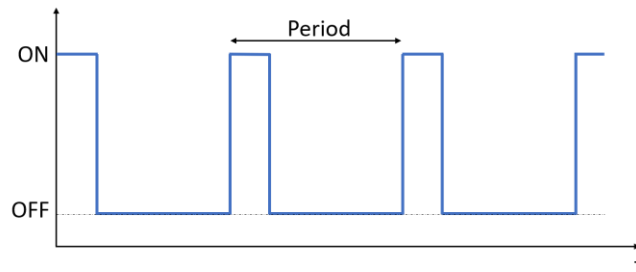
6.605

151.4 Hz

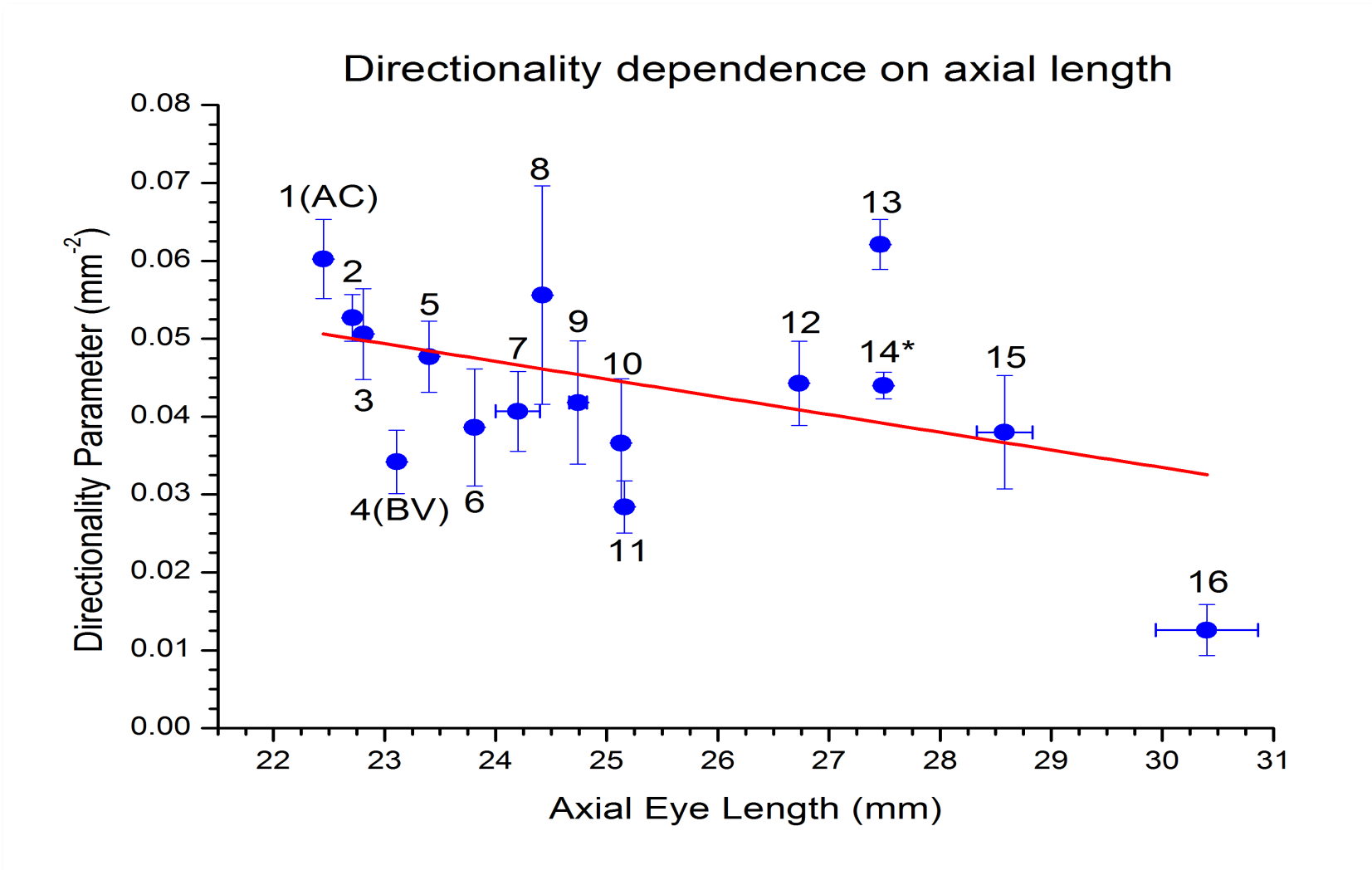
Brighter



Darker



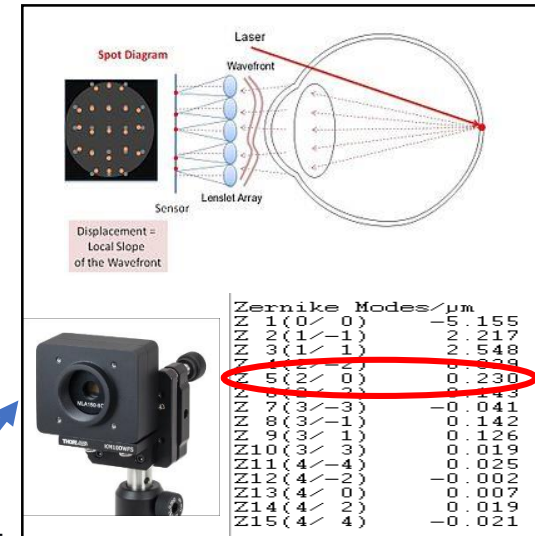
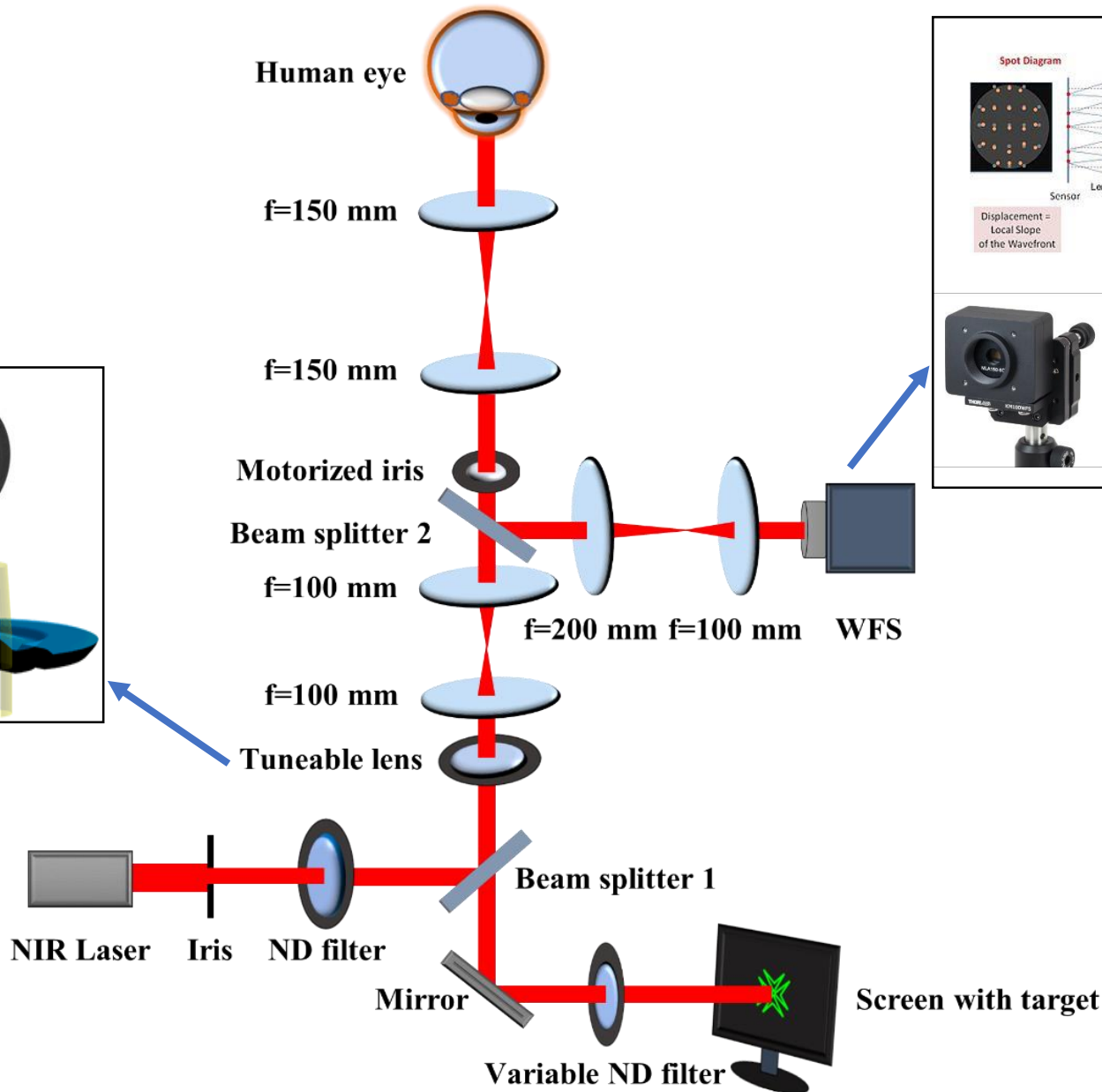
# Reduced directionality = large axial length



Slope:  $-0.002 \pm 0.001 \text{ mm}^{-2}$   
 per  $\text{mm}$  axial length  
 $R^2=0.1796$

$$\rho_M \approx (1 + 2Df_E)\rho$$

# Accommodation and emmetropization



Zernike coefficients

# Altered eye growth in animal models

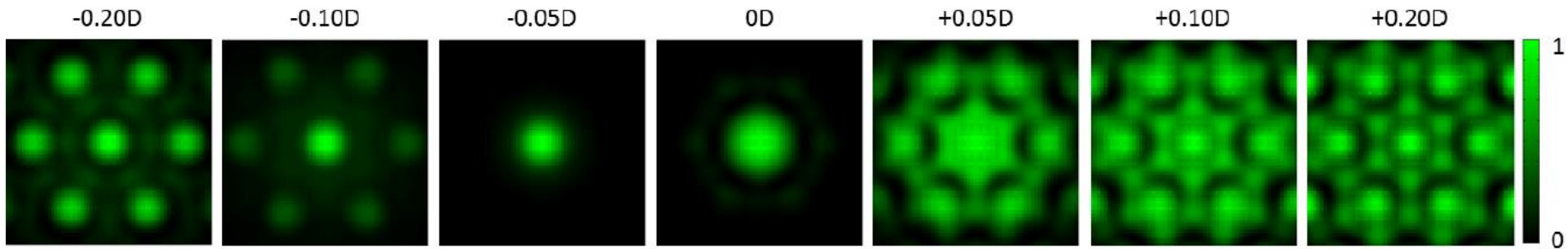
Eye growth can be locally stimulated by local degradation of the retinal image, even after the optic nerve was cut



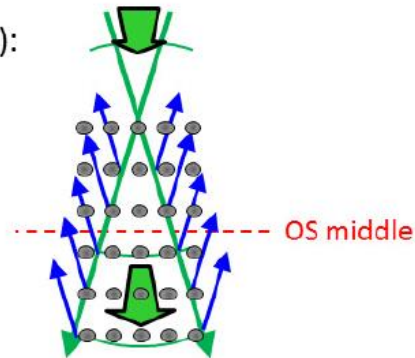
Thus, the retina has at least the complete machinery to convert image features into growth signals.

\*Frank Schaeffel et al, Ophthalmic Physiol Opt 2013, 33, 362–367

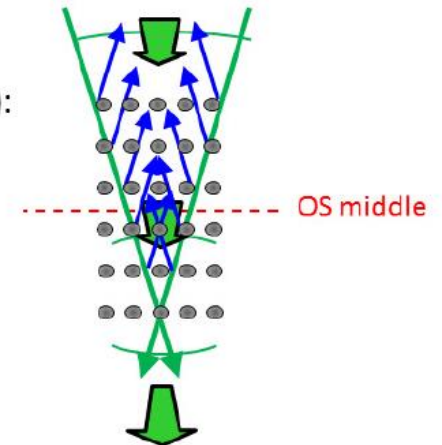
# 3-D retina breaks defocus symmetry



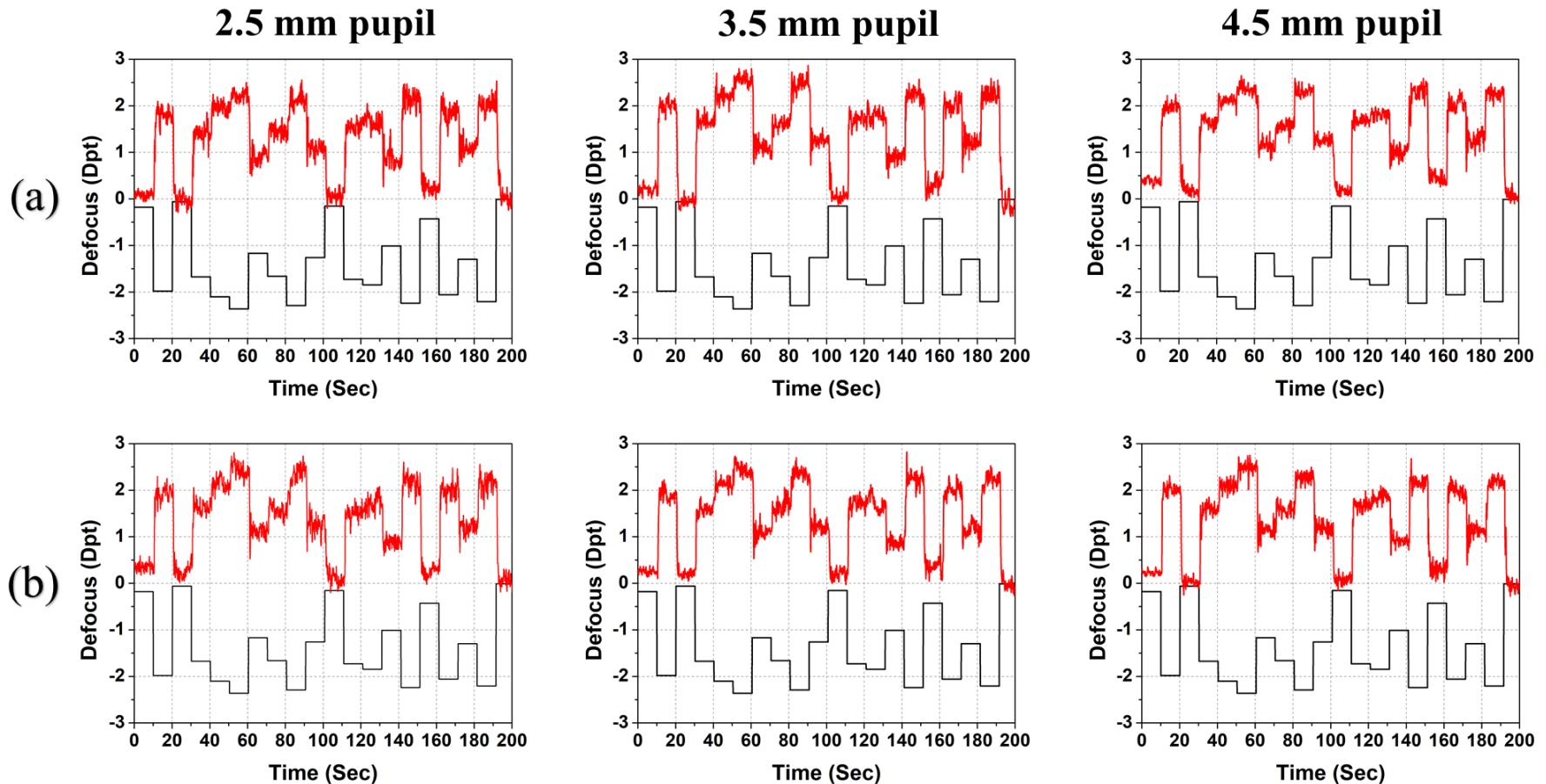
(a) Incident light focused at outer-segment entrance (0D):



(b) Incident light focused at outer-segment exit (-0.05D):

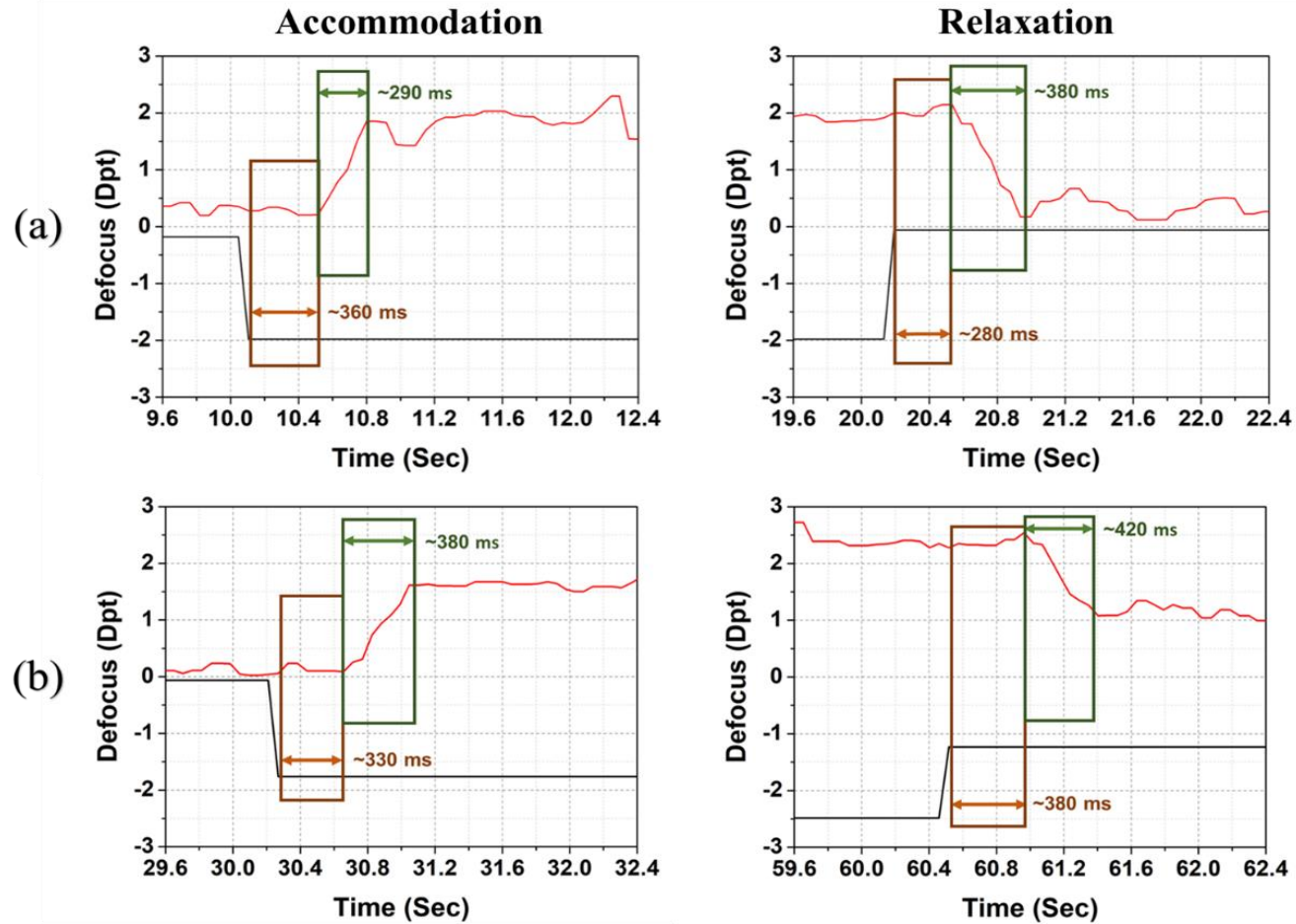


# Temporal response of accommodation



**Test subject (29 years)**

**(a) With and (b) without adjustment of the brightness to compensate changed pupil area**



The **reaction time** was found in the range of **300 – 700 ms** and the **response time 200 – 800 ms**

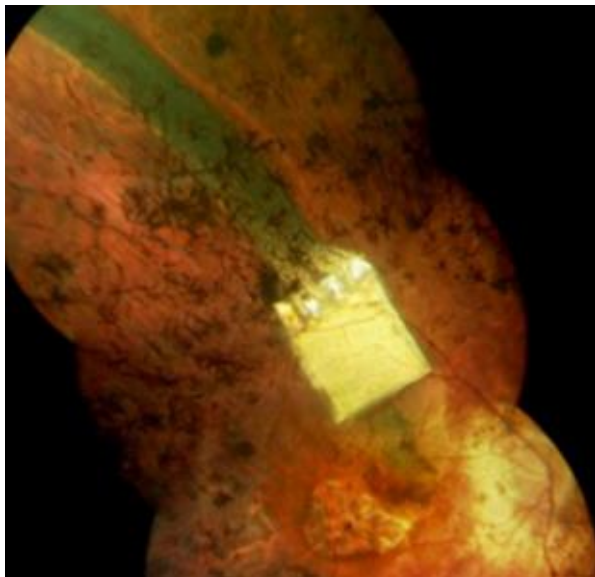
We cannot exclude a neural-triggered response to defocus triggering accommodation



# Towards retinal implants... fighting blindness

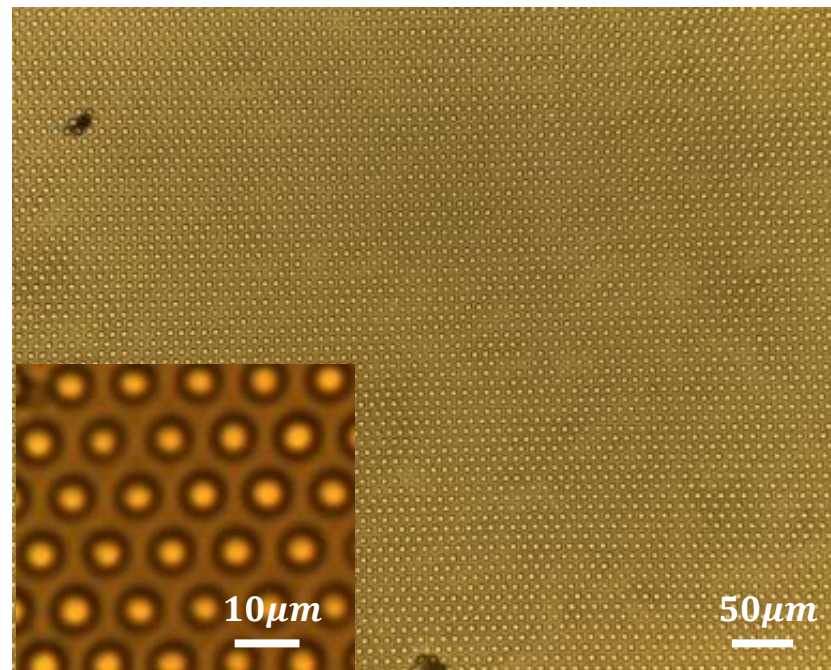
Retinitis Pigmentosa (RP) disease

State-of-the-art implant



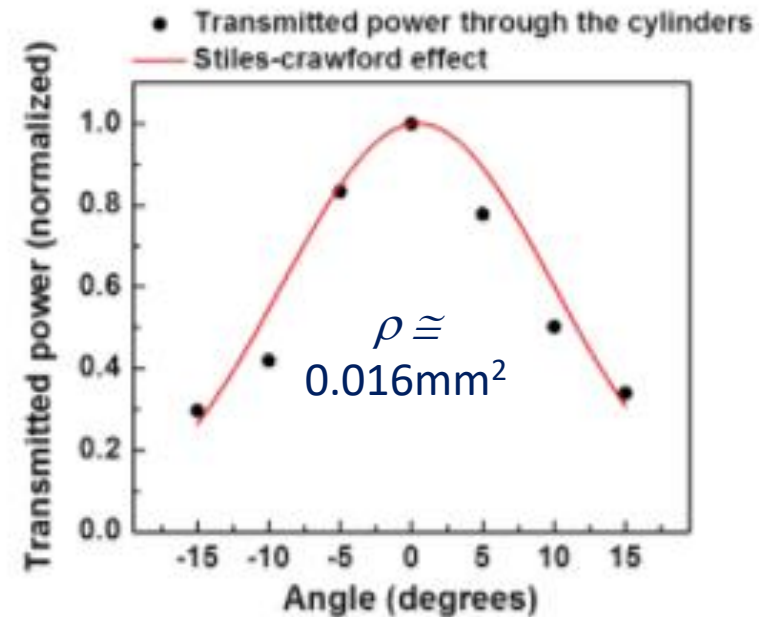
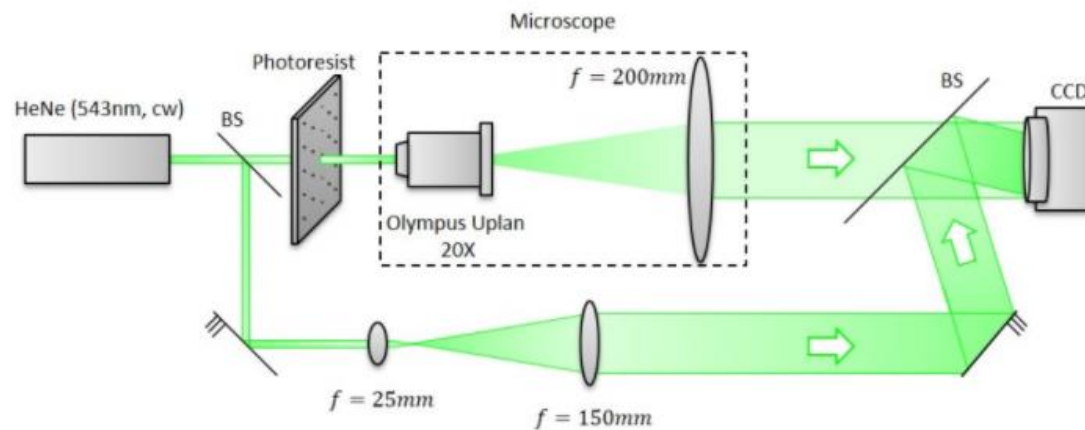
Retinal implant alpha

A retinal simulator in 50 $\mu$ m photoresist AZ40XT



Valente & Vohnsen, Opt. Lett. 2017

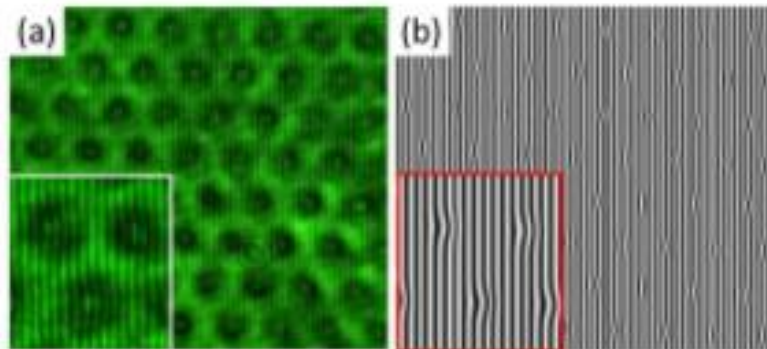
# Retinal simulator model, angular tuning



$$n_{core} = 1.585$$

$$n_{cladd} = 1.581$$

$$d = 5\mu\text{m}$$



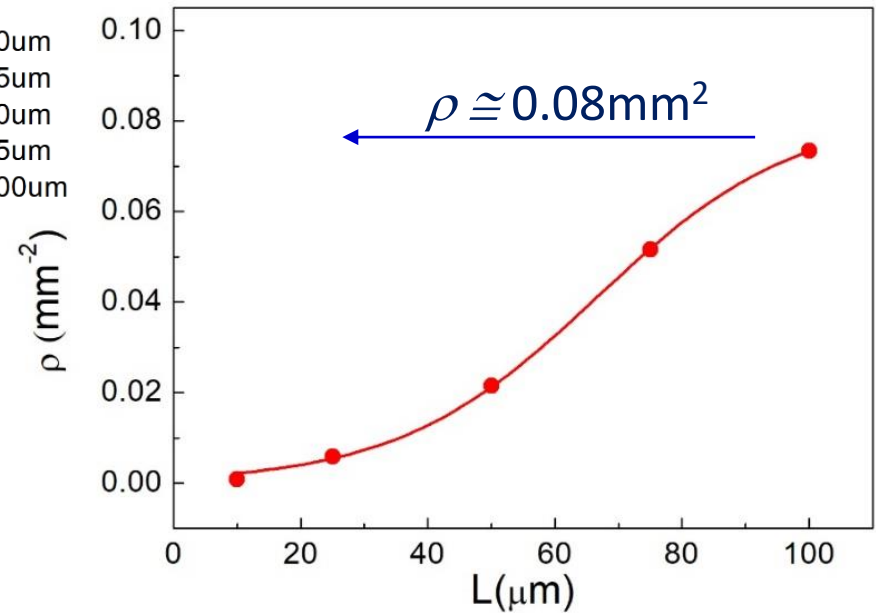
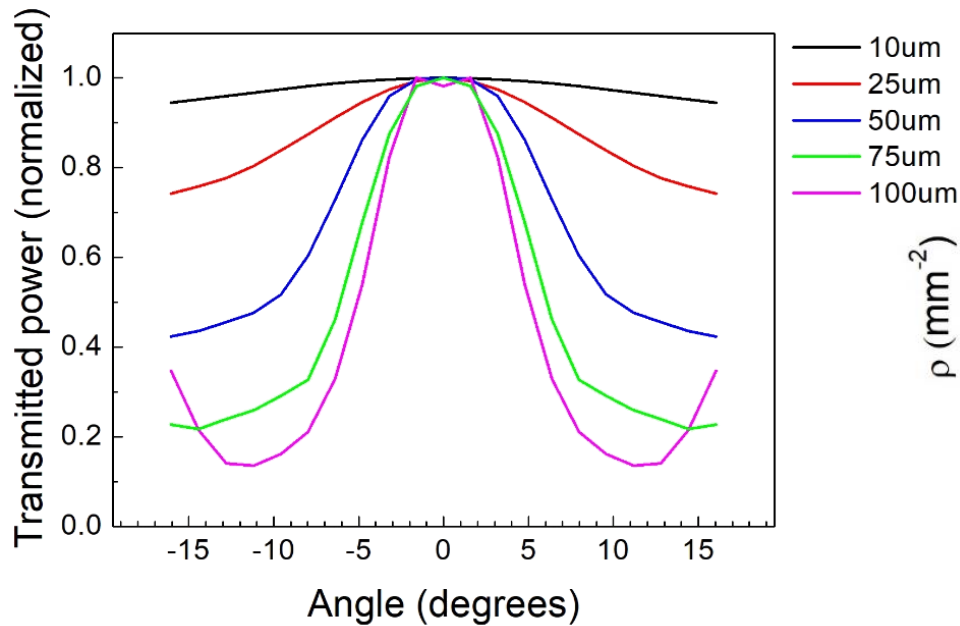
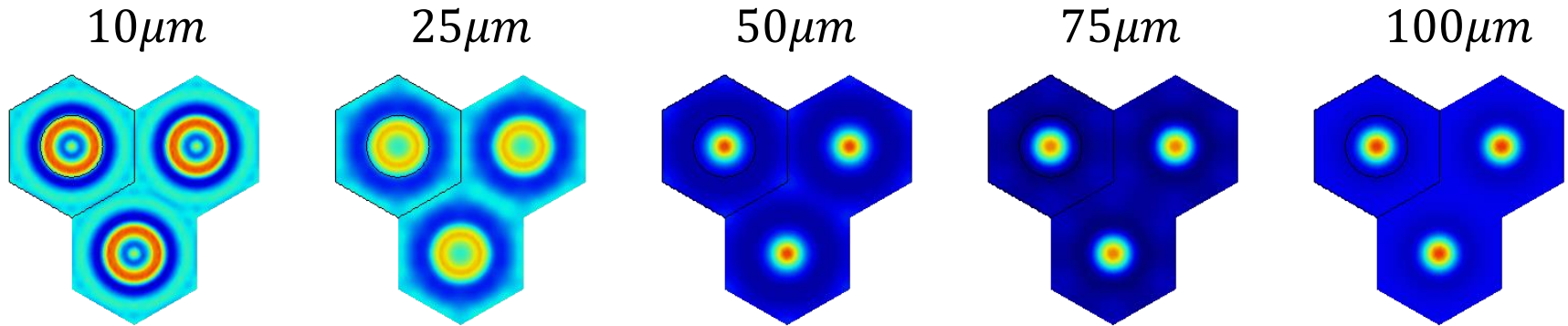
Without printed  
cylinders



With printed  
cylinders



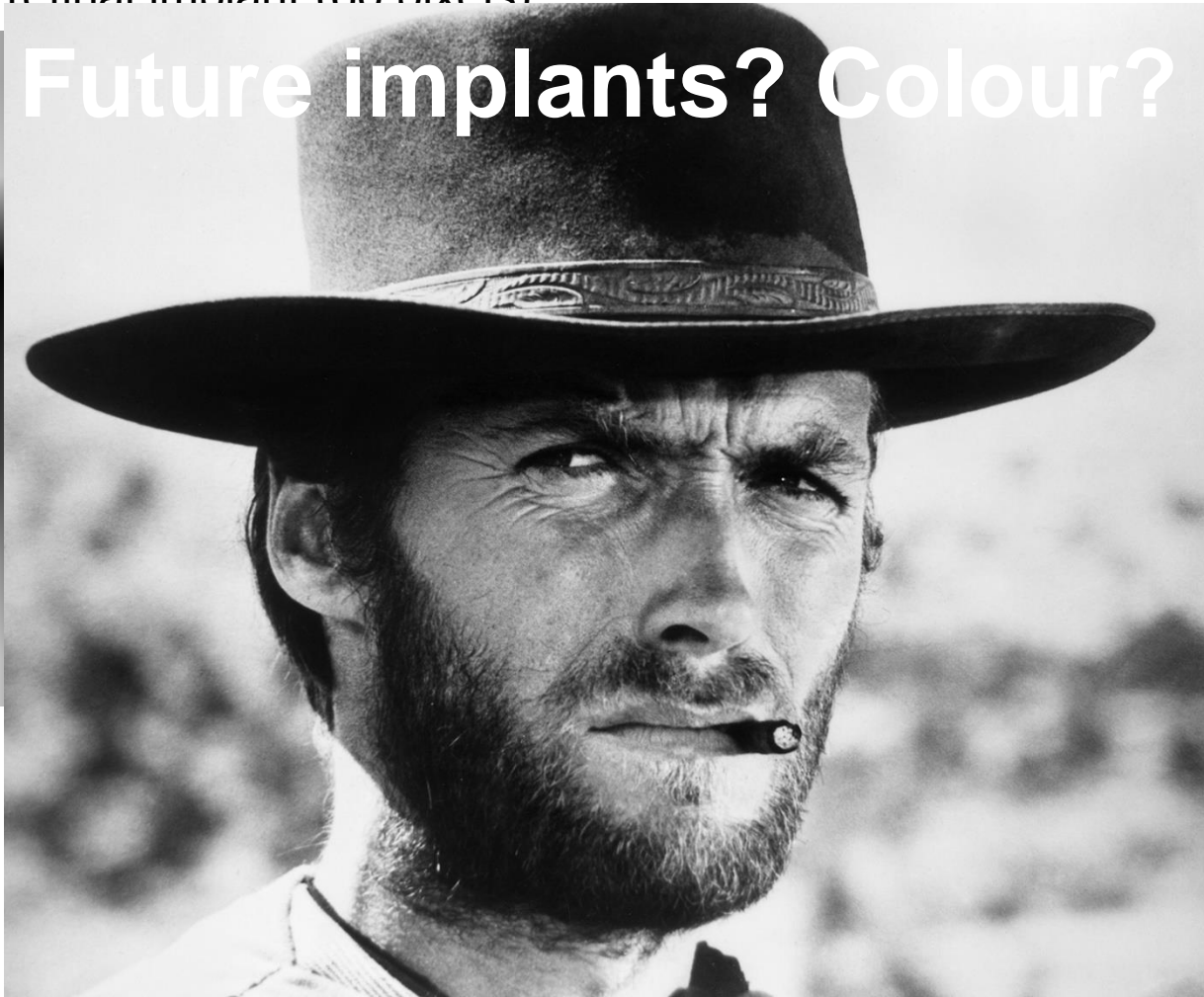
# Photoresist waveguide array, role of waveguide length



# Vision with an implant

Argus II, retinal implant (60 pixels)

Future implants? Colour?

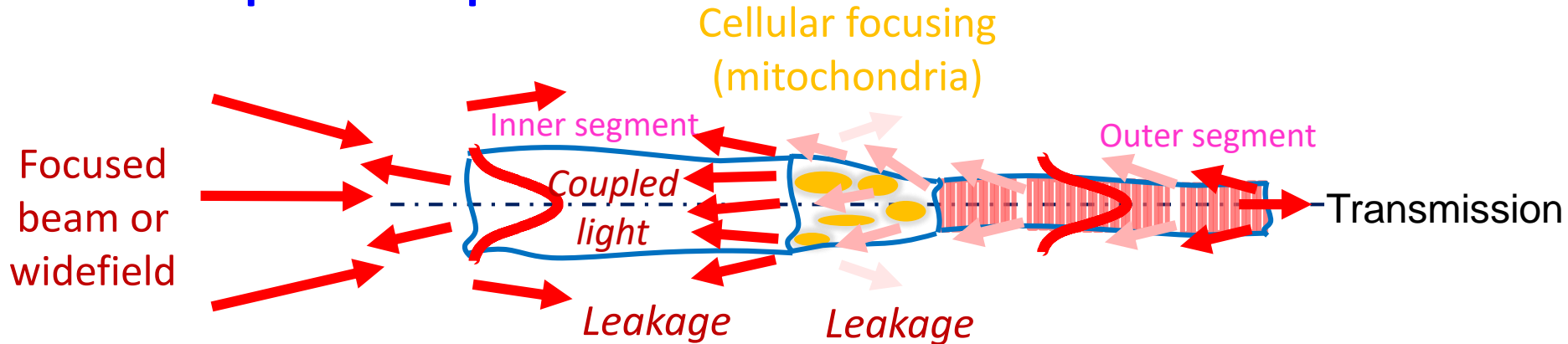


(1500 pixels)



# Directionality when imaging photoreceptors

## Wave-optics interpretation:



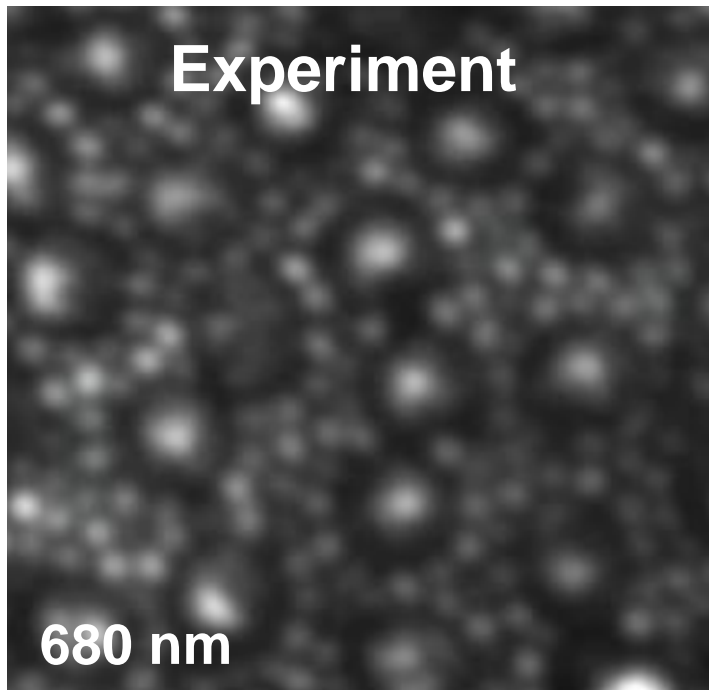
- ❑ Scattering and diffraction from photoreceptors (Vohnsen, BOE 2014)
- ❑ All about refractive index contrast
- ❑ Feature size determines backscattering angle

## Problems?

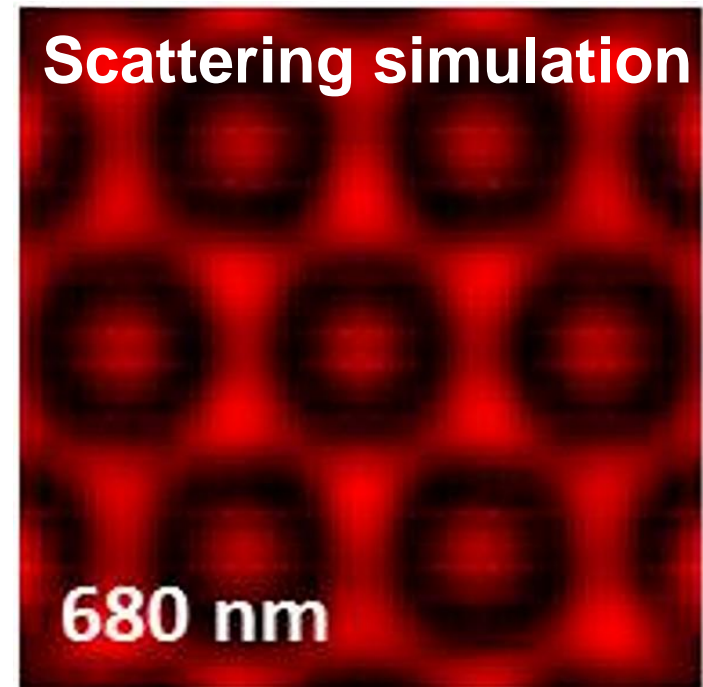
- Impact of densely packed receptors?
- Waveguide and interface variations (beyond  $8^\circ$  no TIR)?
- What *can* be seen, and what *cannot* be seen?

# High resolution retinal imaging

In-vivo cone and rod reflection image by  
courtesy of Alf Dubra (BOE 2011)



Calculated cone mosaic light intensity (no  
rods included) ARVO (Vohnsen, 2014)



Although images are not on the same scale, notice how the dark rings (that form part of the cones) are seen both experimentally and numerically.

# Confocal Scanning Laser Ophthalmoscope

Closed-loop wavefront correction (with a deformable mirror) prior to imaging

## Deformable Mirror (DM)

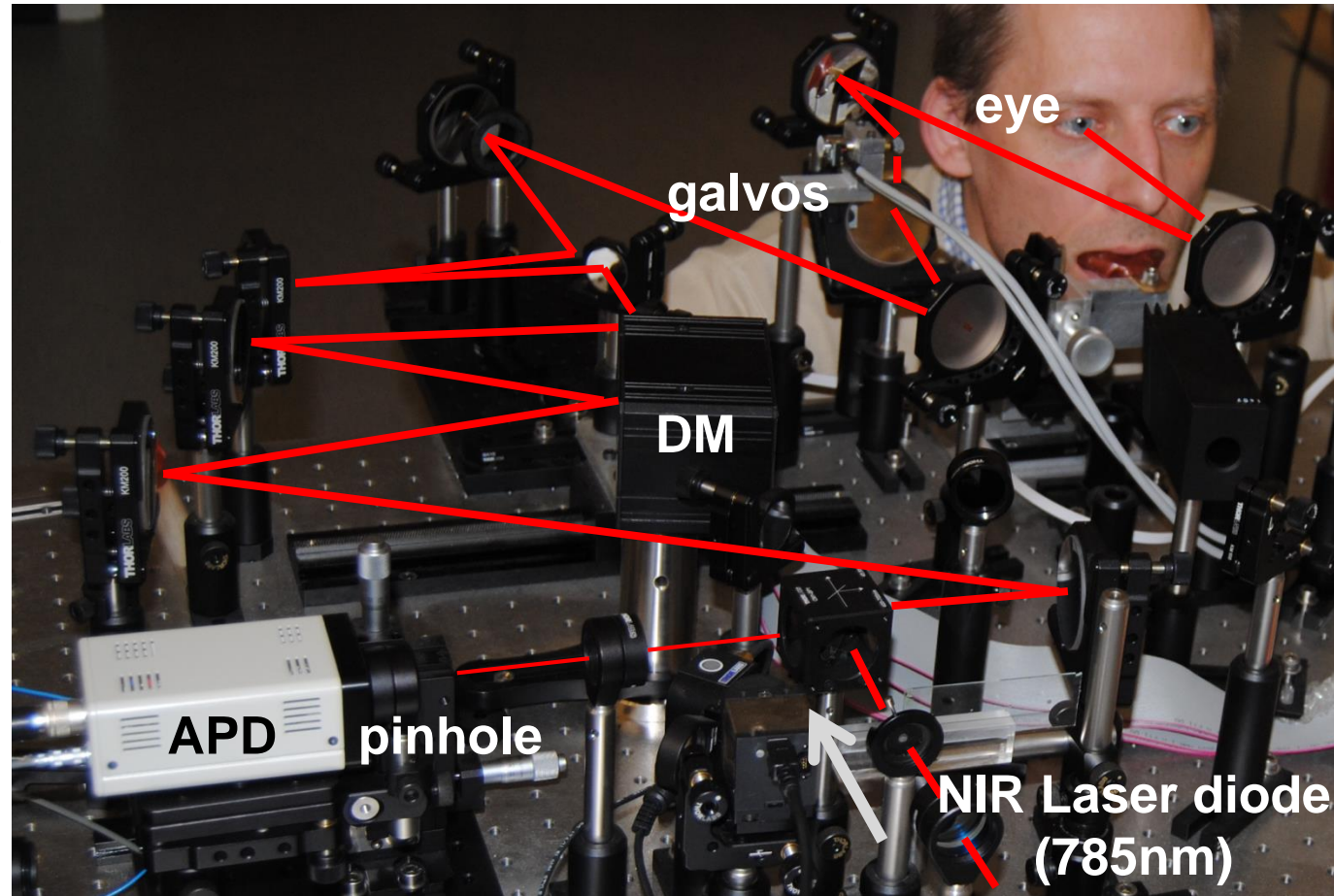
- 140 actuator
- 3.5 micron stroke
- Include 4<sup>th</sup>-order Zernike
- $\varnothing$ 2.5mm (5mm @eye)

## Galvo Scanners

- 12kHz resonant
- 47 fps
- $512 \times 512$  pixels

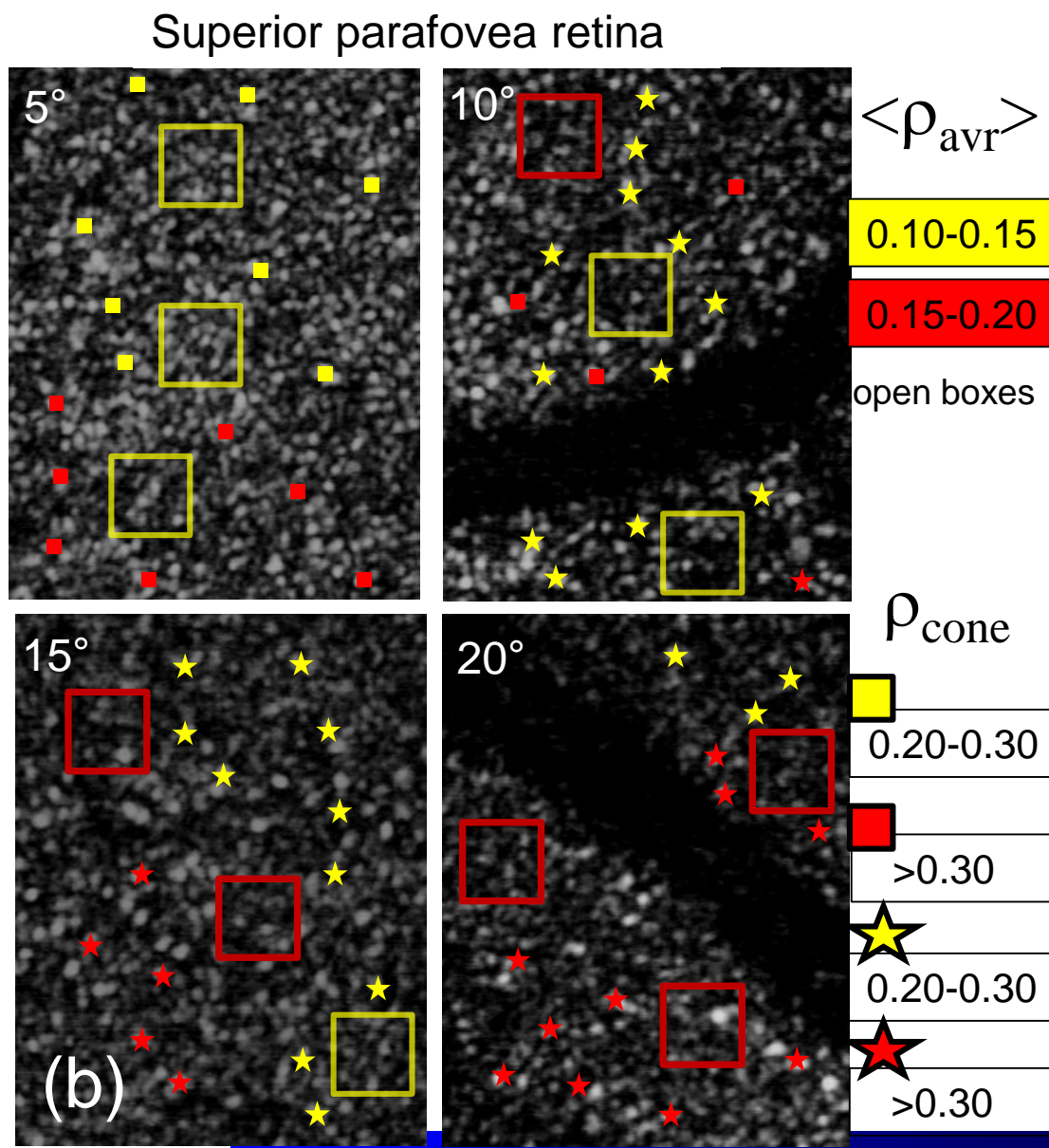
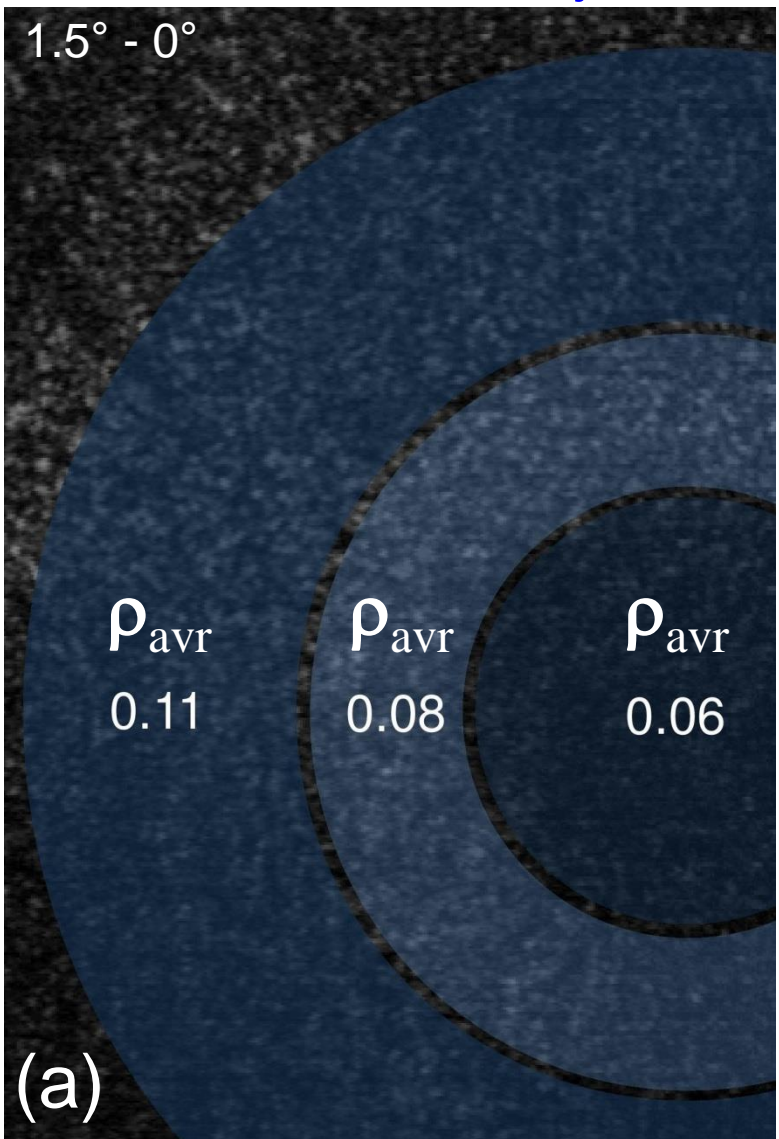
## Detection (APD)

- 75 micron pinhole
- Video signal
- Avalanche photodiode



# SLO-OSCE analysis with pupil sweep of imaging beam

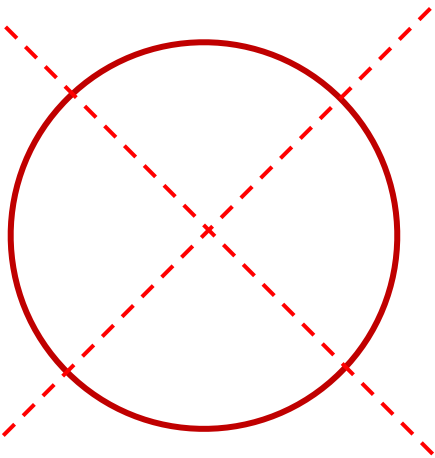
Fovea vicinity **Subject BV**





# Pupil structuring and directional scattering

Splitting the pupil in sectors for simultaneous retinal imaging at different angles



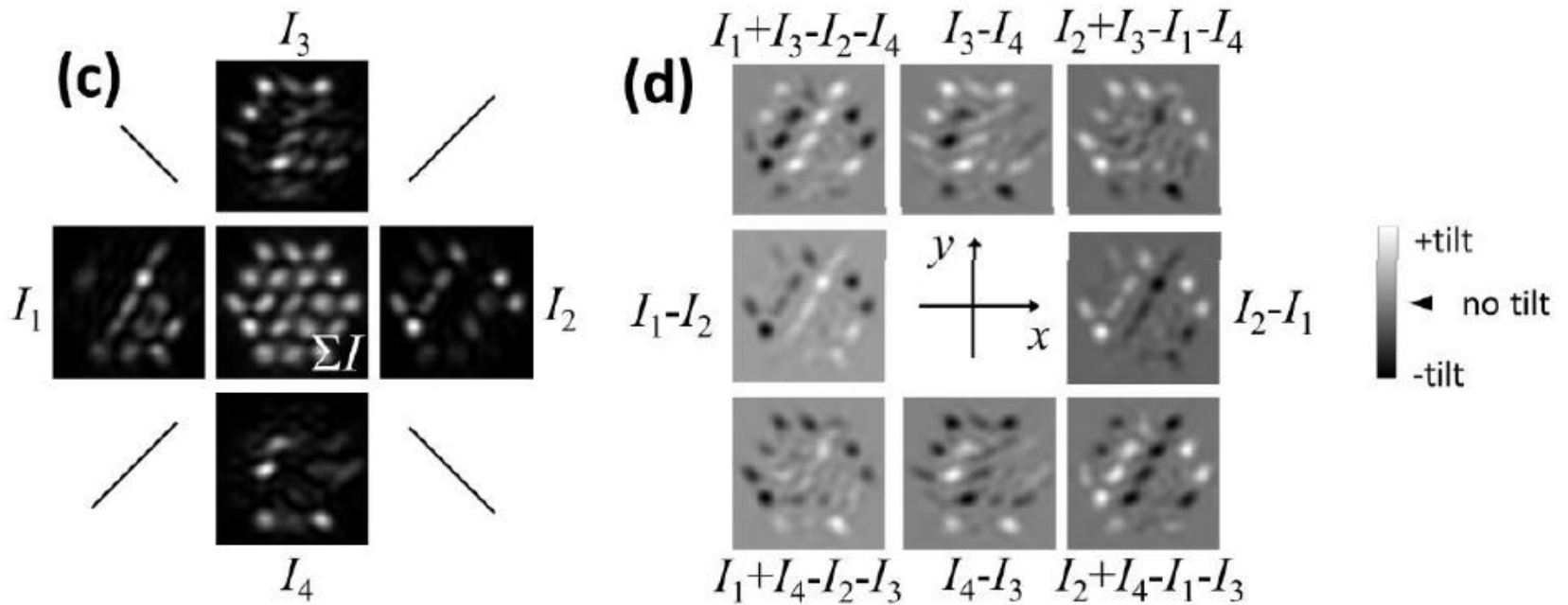
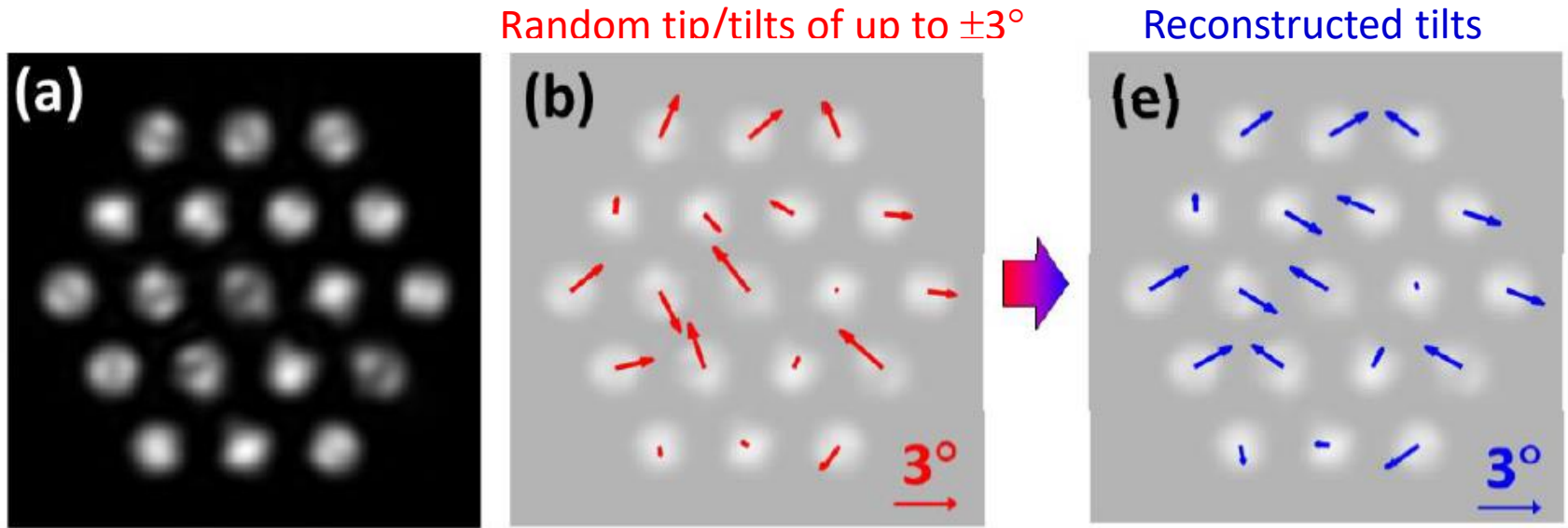
Biomedical Optics Express

Nov. 2018

## Differential detection of retinal directionality

SALIAH QAYSI,<sup>1,\*</sup> DENISE VALENTE,<sup>2</sup> AND BRIAN VOHNSEN<sup>1</sup>

# Cone pointing analysis with an AO fundus camera (model)

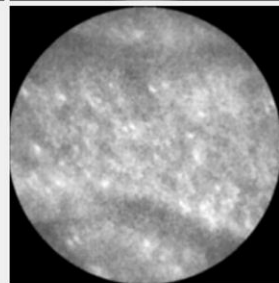
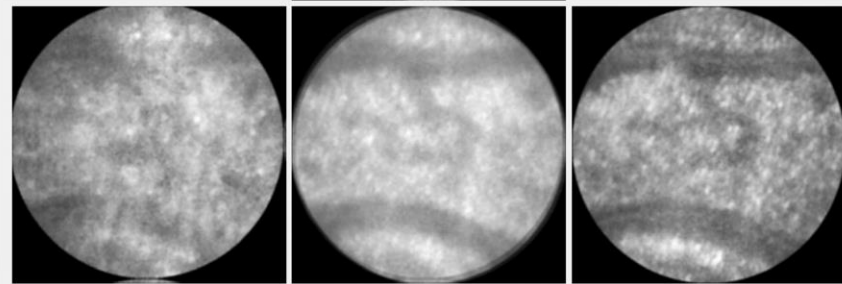
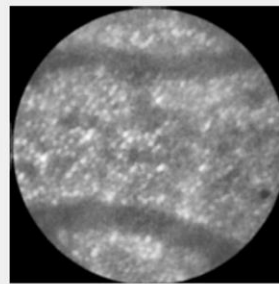


# Pupil-sectored retinal images

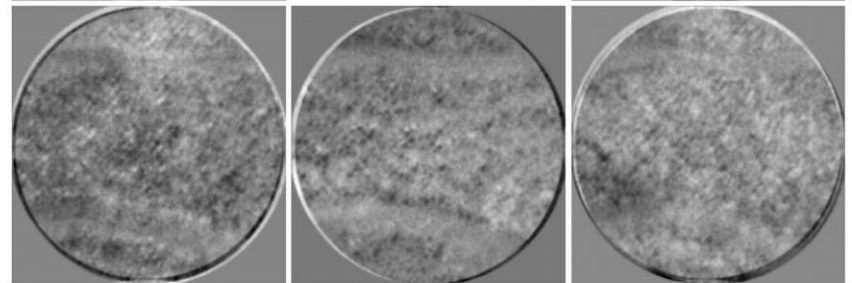
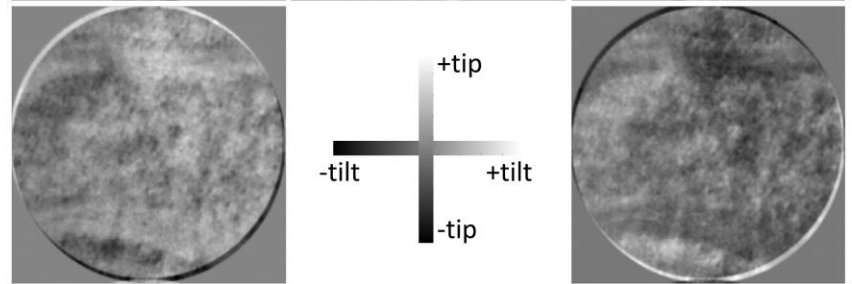
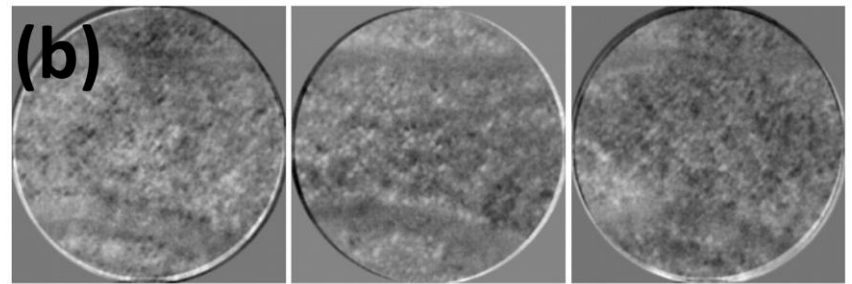
Images

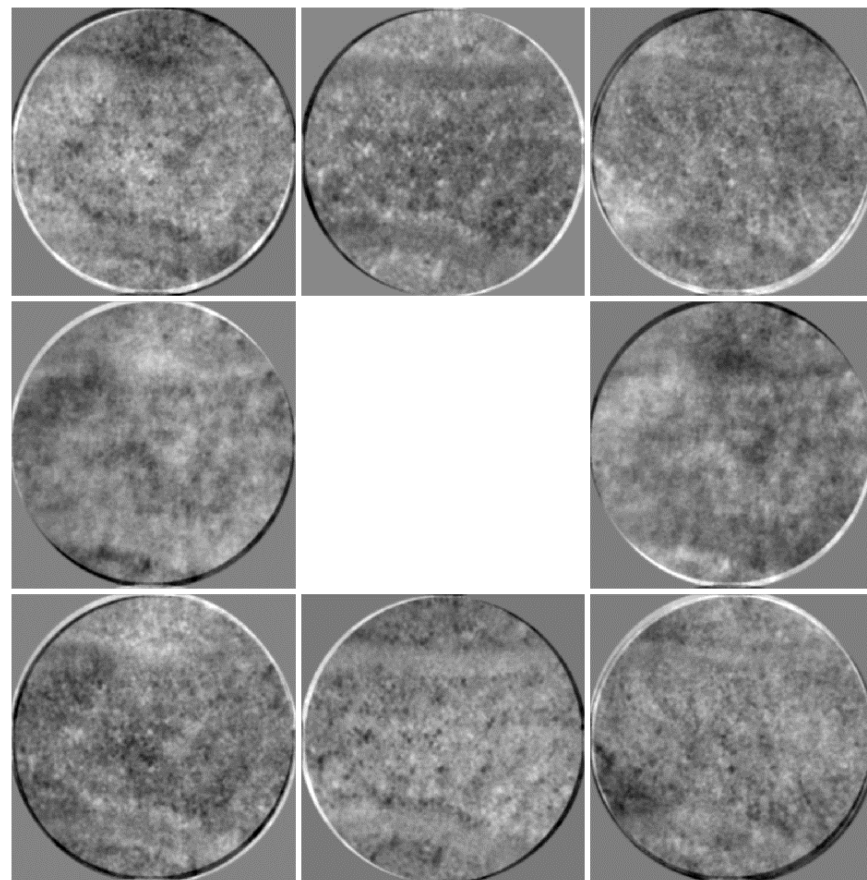
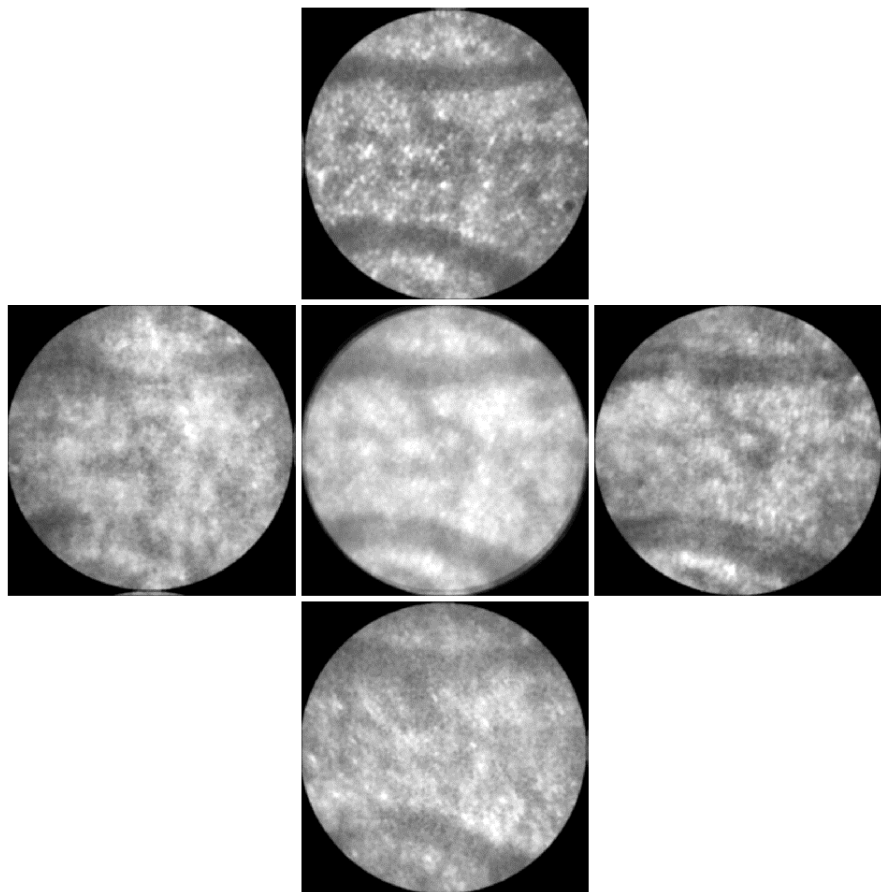
Difference images

(a)



(b)





# Local inclination vector at each pixel (m,n)

Inclination vector at pixel (m,n)

$$\Delta x_{m,n} = \frac{I_{2,m,n} - I_{1,m,n}}{I_{2,m,n} + I_{1,m,n}} L \quad ; \quad \Delta y_{m,n} = \frac{I_{3,m,n} - I_{4,m,n}}{I_{3,m,n} + I_{4,m,n}} L$$

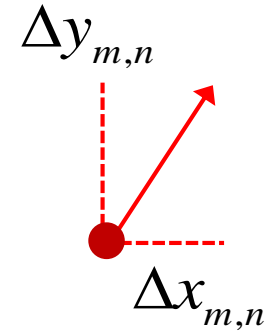
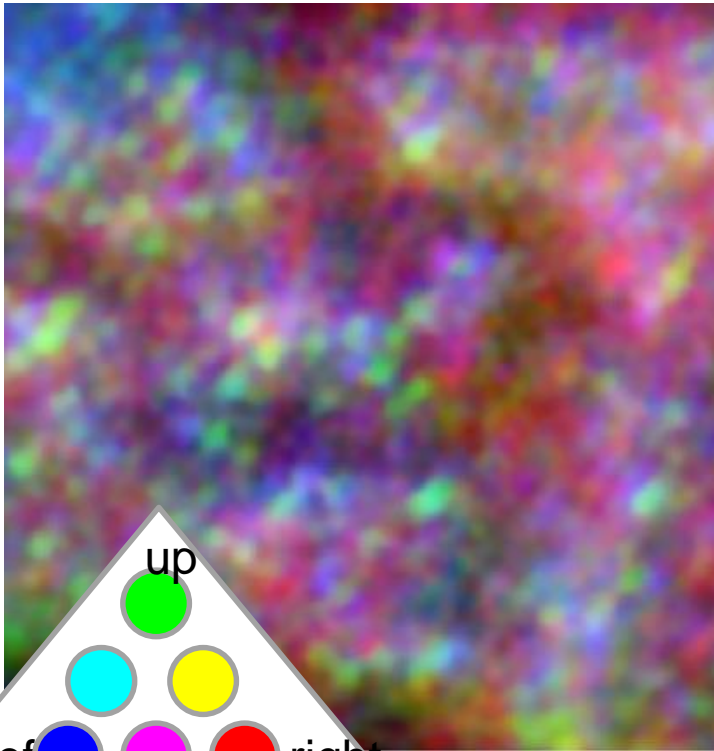


Image inclination metric (N x N pixels)

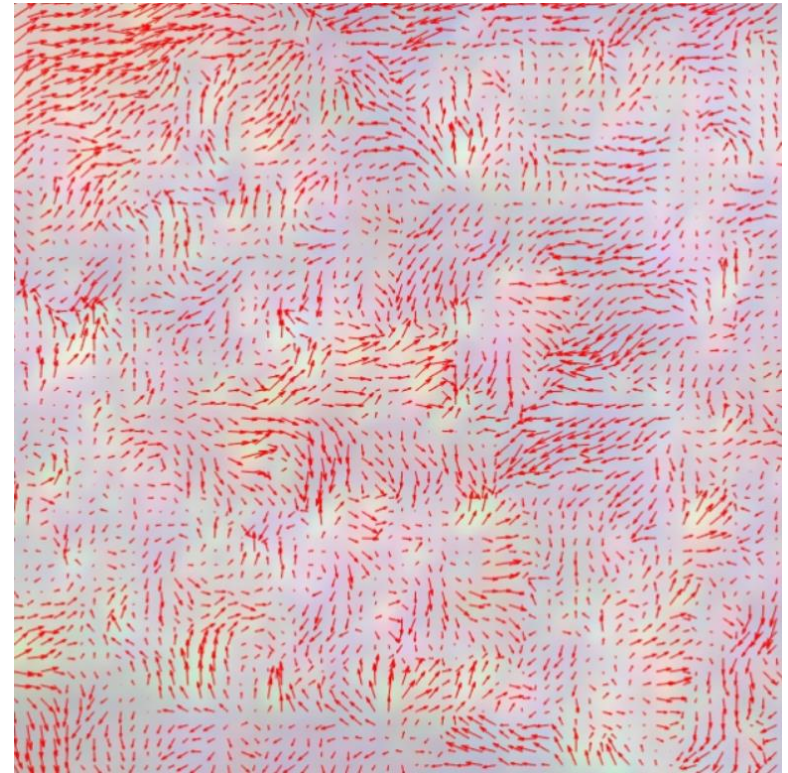
$$\sigma = \frac{1}{\sqrt{2}N^2} \sum_{n=1}^N \sum_{m=1}^N \sqrt{(\Delta x_{m,n} / L)^2 + (\Delta y_{m,n} / L)^2}$$

# Cones with local inclination vectors

Colour-coded parafoveal cone mosaic

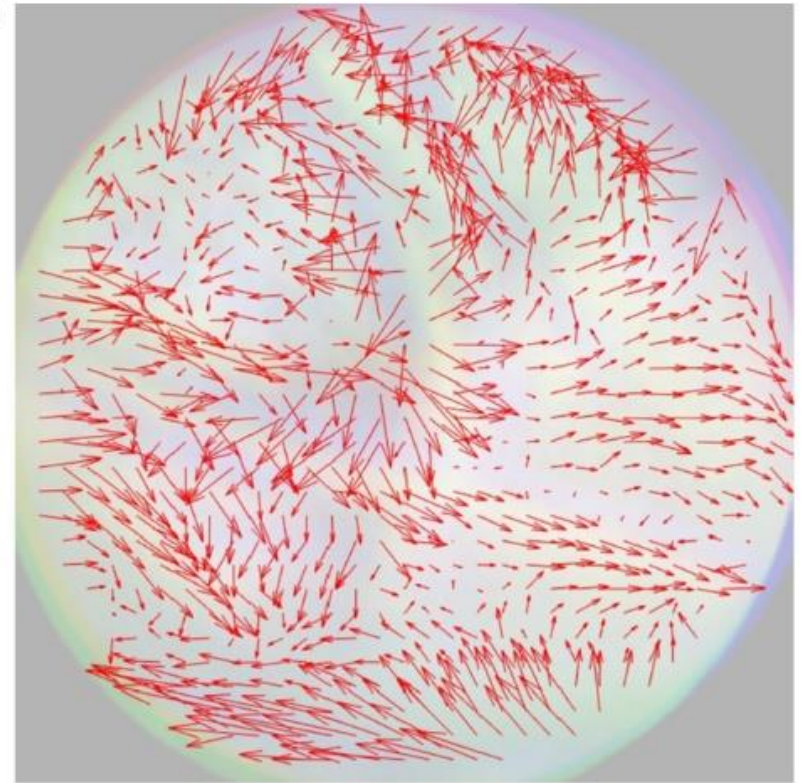
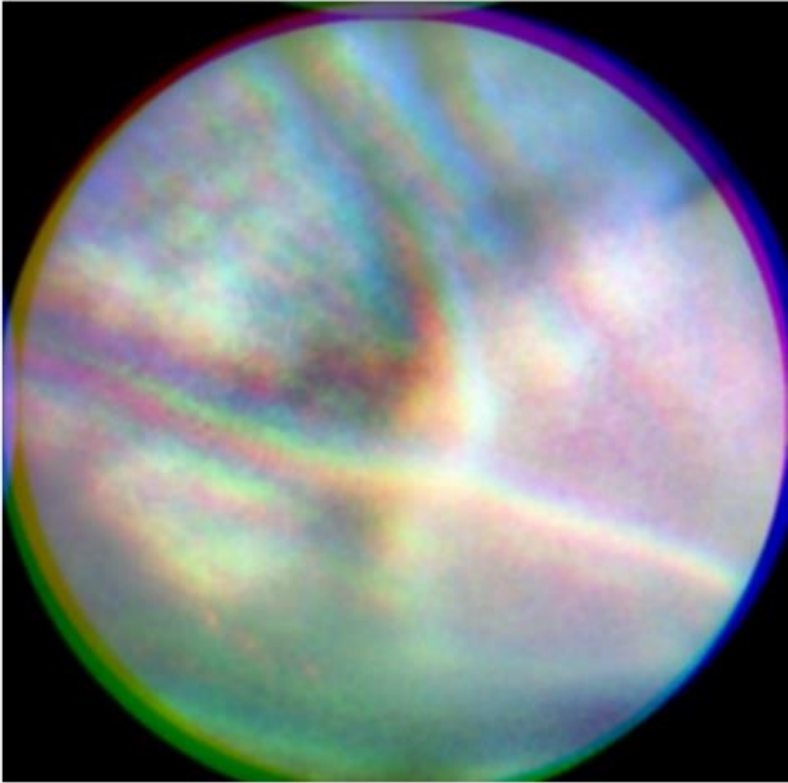


Vector inclination plot



$$\sigma = 0.091$$

# Colour coding and inclination near the optic disc



$$\sigma = 0.090$$

# Conclusions

- A volumetric absorption model gives good estimates for the SCE-I and for the integrated Stiles-Crawford effect
- Electromagnetic absorption model gives fair estimates for the SCE-I, and may explain rod directionality due to dense absorption in rhodopsin
- Scattering calculations can produce simulated images that may help interpret experimental results
- Directional retinal scattering can be analysed with differential analysis as demonstrated with an AO-fundus camera



# Acknowledgments

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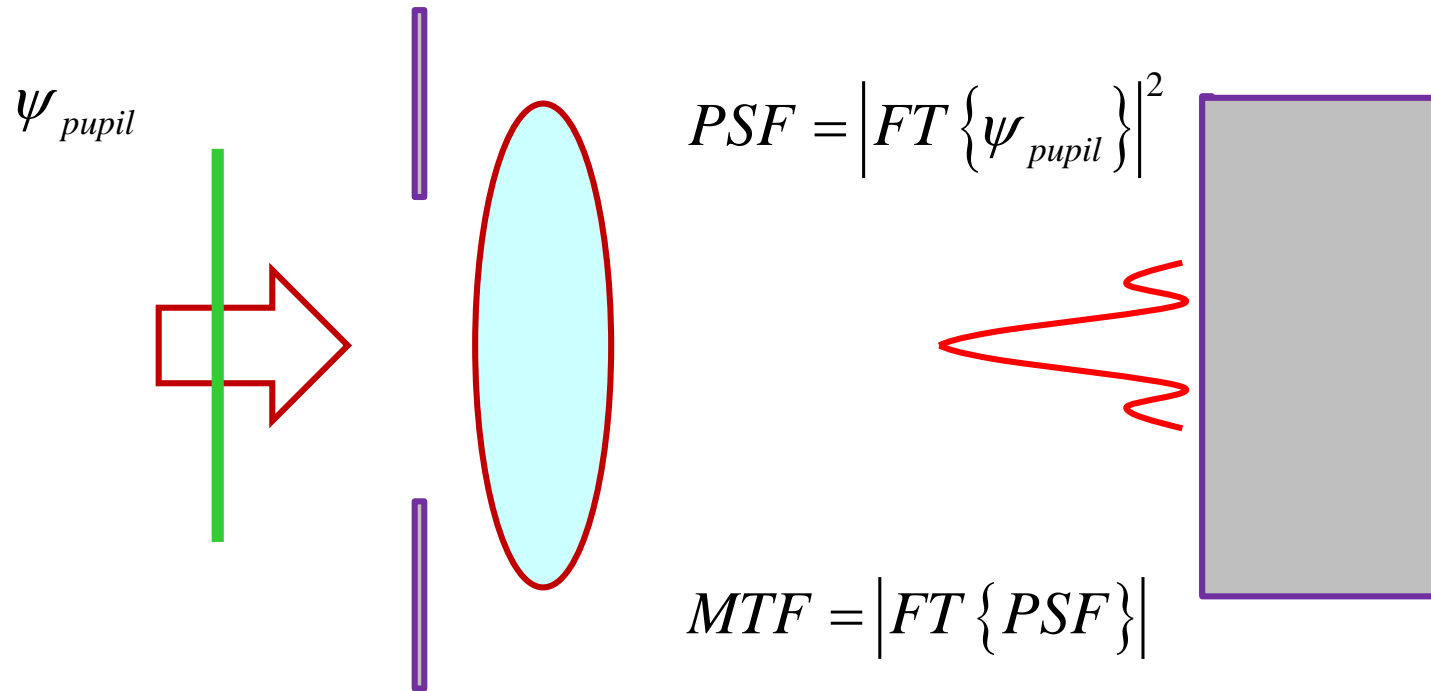


King Abdullah Scholarships  
Program



[brian.vohnsen@ucd.ie](mailto:brian.vohnsen@ucd.ie)

# PSF and MTF (**mis-**)concepts



Depth-of-focus  $DOF = 8\lambda f^2 / d^2$

...at best these are **1<sup>st</sup>-order approximations**